

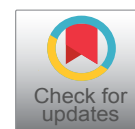


REVIEW ARTICLE

Pharmaceutical Particle Engineering via Nano Spray Drying - Process Parameters and Application Examples on the Laboratory-Scale

Cordin Arpagaus*

NTB University of Applied Sciences of Technology Buchs, Institute for Energy Systems, Switzerland



*Corresponding author: Arpagaus Cordin, NTB University of Applied Sciences of Technology Buchs, Institute for Energy Systems, Erdenbergstrasse 4, 9471 Buchs, Switzerland, Tel: +41-81-755-34-94, E-mail: cordin.arpagaus@ntb.ch

Abstract

Spray drying plays a crucial role in the processing of pharmaceutical products such as pills, capsules, and tablets as it is used to convert drug-containing liquids into dried powdered forms. Nano spray drying is in particular used to improve drug formulation by encapsulating active ingredients in polymeric wall materials for protection and delivering the drugs to the right place and time in the body. The nano spray dryer developed in the recent years extends the spectrum of produced powder particles to the submicron- and nanoscale with very narrow size distributions and sample quantities in the milligram scale at high product yields. This enables the economical use of expensive active pharmaceutical ingredients and pure drugs. The present paper explains the concept of nano spray drying in the laboratory-scale and discusses the influence of the main process parameters on the final powder properties like particle size, morphology, encapsulation efficiency, and drug loading. Application results of nano spray drying for the formulation and encapsulation of different drugs are reviewed.

Keywords

Nano spray drying, Pharmaceuticals, Drug encapsulation, Particle size, Powder

ceutical industry. Table 1 lists some examples of marketed pharmaceutical products processed by spray drying technology [2-8].

Typically, the drug is dissolved in a polymeric carrier solution and atomized into hot gas to evaporate the solvent, resulting in particles containing the drug dispersed in an amorphous polymer matrix [9]. Polymers such as hydroxypropyl methylcellulose or its acetate succinate have become the first choice for the preparation of stable solid dispersions as they are resistant to water absorption [3]. A few spray-dried pharmaceutical products are on the market for inhalation therapies. In 2013, the US Food and Drug Administration approved Novartis TOBI® Podhaler™ with 28 mg Tobramycin inhalation powder per capsule for the treatment of cystic fibrosis patients with *Pseudomonas aeruginosa* bacteria in the lungs. The Tobramycin inhalation powder is manufactured using PulmoSphere™ technology, an emulsion-based spray drying process that produces spherical hollow-porous particles (Figure 1).

Introduction

Spray drying is a simple, fast, continuous, and scalable drying technology that is well established in the pharmaceutical industry for excipient production, microencapsulation, or granulation [1]. Many pharmaceutical products such as pills, capsules, and tablets are processed in dried powdered form. Progress was made in introducing spray-drying technology to the pharma-

The dried particles have a geometric mean diameter of about 1 to 2.7 μm and a mean mass diameter of $< 4 \mu\text{m}$, which is ideal for delivering the drug to the lower respiratory [5,6]. Spray dried powder consists of 28 mg Tobramycin active ingredient with distearoylphosphatidylcholine calcium chloride and sulfuric acid for pH adjustment. The drug is packaged in a hypromellose capsule containing 28 mg of active ingredient each. The capsules are stored individually



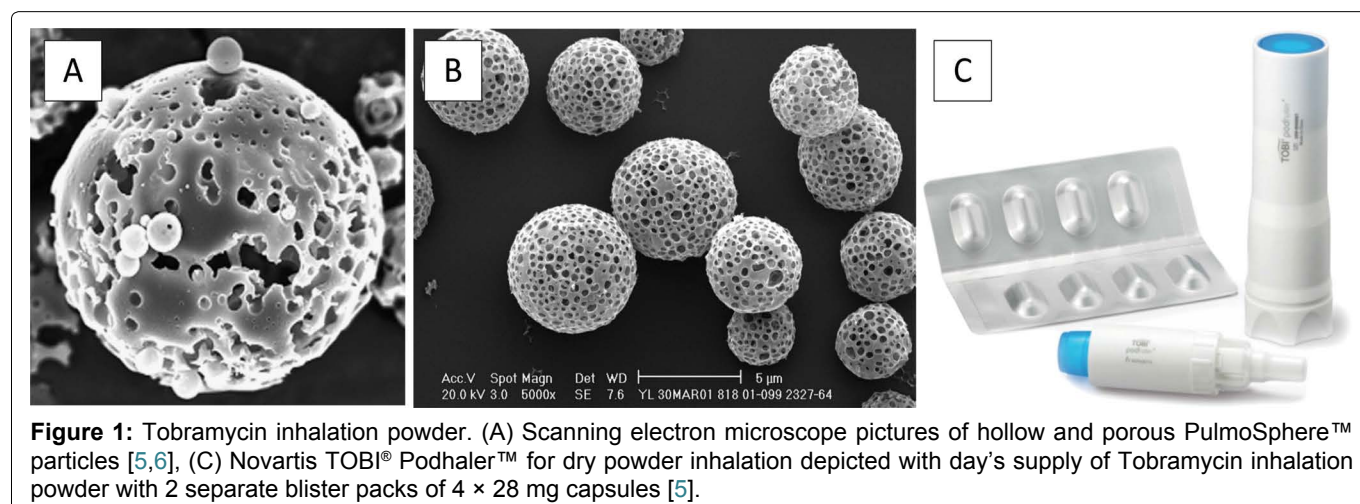
Citation: Arpagaus C (2018) Pharmaceutical Particle Engineering via Nano Spray Drying - Process Parameters and Application Examples on the Laboratory-Scale. Int J Med Nano Res 5:026. doi.org/10.23937/2378-3664/1410026

Accepted: December 03, 2018; **Published:** December 05, 2018

Copyright: © 2018 Arpagaus C. This is an open-access article distributed under the terms of the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original author and source are credited.

Table 1: Examples of FDA-approved medicaments that use spray drying technology as preparation method. HPMC: Hydroxypropyl Methylcellulose; HPMCAS: Hydroxypropyl Methylcellulose Acetate Succinate; DSPC: Distear-ylphosphatidylcholine (data summarized from [2-8]).

Trade name	Drug	Application	Polymer, Excipient	Maximum drug dose	Company	FDA approval
Prograf	Tacrolimus	Immunosuppressant (prevents organ rejection)	HPMC	5 mg per capsule	Astellas Pharma	1994
Exhubera	Insulin	Diabetes	Mannitol, glycine, sodium citrate	1 or 3 mg per capsule	Pfizer/Nektar	2006
Intelence	Etravirine	HIV medicine	HPMC	100 or 200 mg per tablet	Janssen	2008
Zortress	Everolimus	Immunosuppressant (prevents organ rejection)	HPMC	0.75 mg per tablet	Novartis	2010
Aridol/Osmohale, Bronchitol	-	Asthma/ Cystic fibrosis	Mannitol	5 to 40 mg per capsule	Pharmaxis	2010
Incivek	Telaprevir	Hepatitis C	HPMCAS	375 mg per tablet	Vertex	2011
Kalydeco	Ivacaftor	Cystic fibrosis	HPMCAS	150 mg per tablet	Vertex	2012
TOBI Podhaler	Tobramycin	Inhalation therapy	DSPC, calcium chloride, sulfuric acid	28 mg per capsule	Novartis	2013
Raplixa	-	Bleeding control during surgery	Fibrinogen/Thrombin	79 mg/726 IU per gram powder	Nova Laboratories	2016



in aluminum blister packs of four to protect them from moisture in the environment. Pharmaxis commercialized spray dried inhalable mannitol (sugar alcohol) powders Aridol/Osmohale™ and Bronchitol™ in 2011 and 2012 for diagnosis of asthma by detecting active airway inflammation through measuring bronchial hyper-responsiveness [7]. Mannitol is crystalline after spray drying and physically stable due to its low glass transition temperature. It rehydrates the airway/lung surface and promotes a productive cough. Bronchitol dry powder helps to increase mucus clearance and improves the lung function and the quality of life of people living with cystic fibrosis.

Already in 2006, Exhubera® (Pfizer/Nektar Therapeutics) became the first inhaled human insulin approved for use in type 1 or type 2 diabetes [8]. Exhubera powder was prepared by spray drying 60% recombinant human insulin mixed with glycine, mannitol, and sodium citrate as stabilizers. The spray dried powders exhibited good flowability, low moisture content, and good

storage stability at room temperature. The aerosolized insulin had a mass median aerodynamic diameter of approximately 3 μm. The spray-dried insulin powder was packaged in blisters containing 1 mg or 3 mg of insulin. Despite the promise of a new delivery system, Exhubera was not profitable in the insulin market and the product was withdrawn in 2007 because of low sales. New strategies for the administration of inhaled insulin are being further investigated.

In May 2015, the FDA approved Raplixa, the first sterile, spray dried fibrin seal powder used to control adult bleeding during surgery [8]. The powder is applied to the sampling site directly from the vial or by using a low-pressure spray device. The fibrin sealant then dissolves in the blood and begins to clot the blood. Raplixa comprises spray-dried thrombin and spray-dried fibrinogen, which are aseptically mixed and filled into a single vial. Each gram of Raplixa contains 79 mg fibrinogen and 726 IU thrombin. This eliminates the need to combine fibrinogen and thrombin before use

and the product can be stored at room temperature. Commercial supplies of Raplixa sealing powder are produced at the sterile production facilities of Nova Laboratories by aseptic spray drying.

From a technological point of view spray drying offers flexibility in particle formulation. By tuning the spray drying parameters, it is possible to manipulate the particle properties, e.g. particle size, shape, morphology, surface roughness, or surface composition.

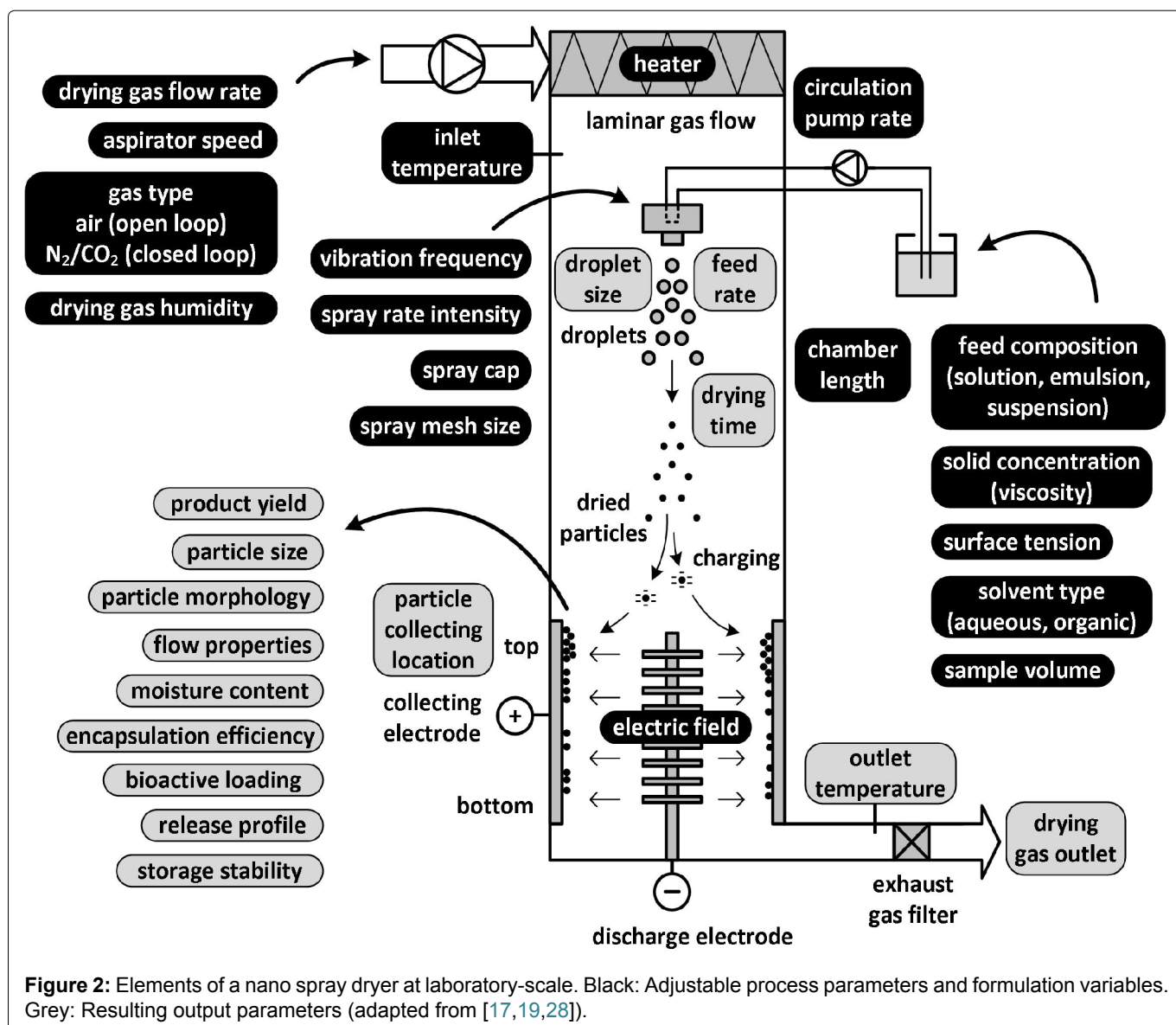
In the course of the rapid progress of nanoencapsulation techniques, nano spray drying technology has also developed, in particular at Buchi Labortechnik AG (Switzerland), with the development of the Nano Spray Dryer B-90 [10-14]. The laboratory-scale nano spray dryer enables the formulation of drugs with solid colloidal particles in the submicron range. Detailed information on the formation of nanocapsules by the nano spray drying technology can be found in several review studies [10-24], in particular in a recently published book chapter and review paper by Arpagaus et al. [17,19]. The term nanoparticle in the pharmaceutical industry is typically defined as solid colloidal particles with sizes below 1 μm

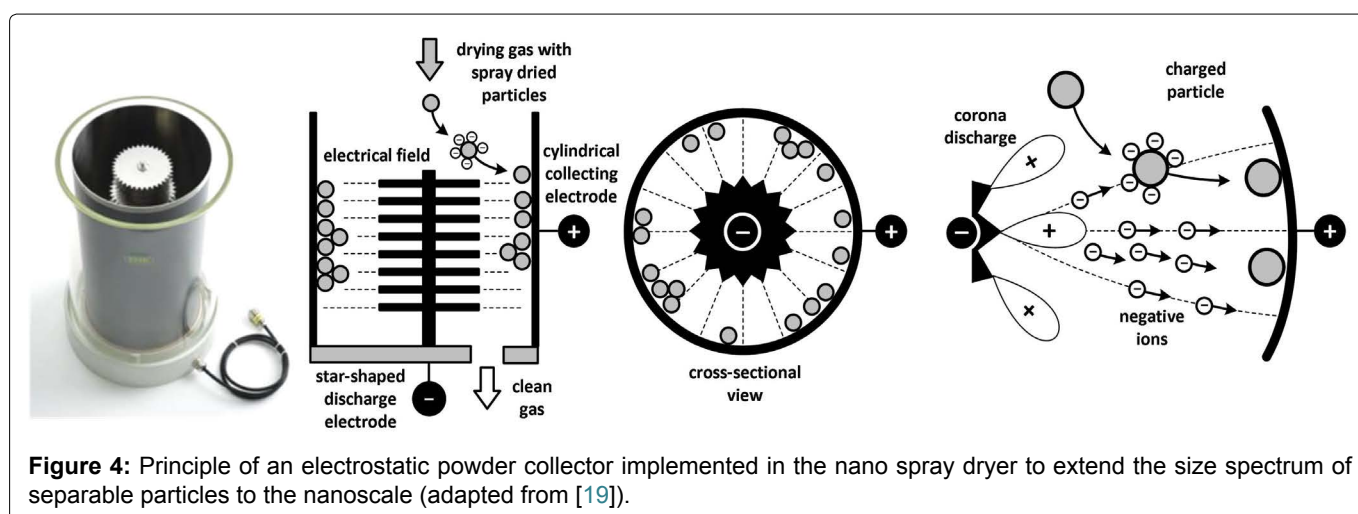
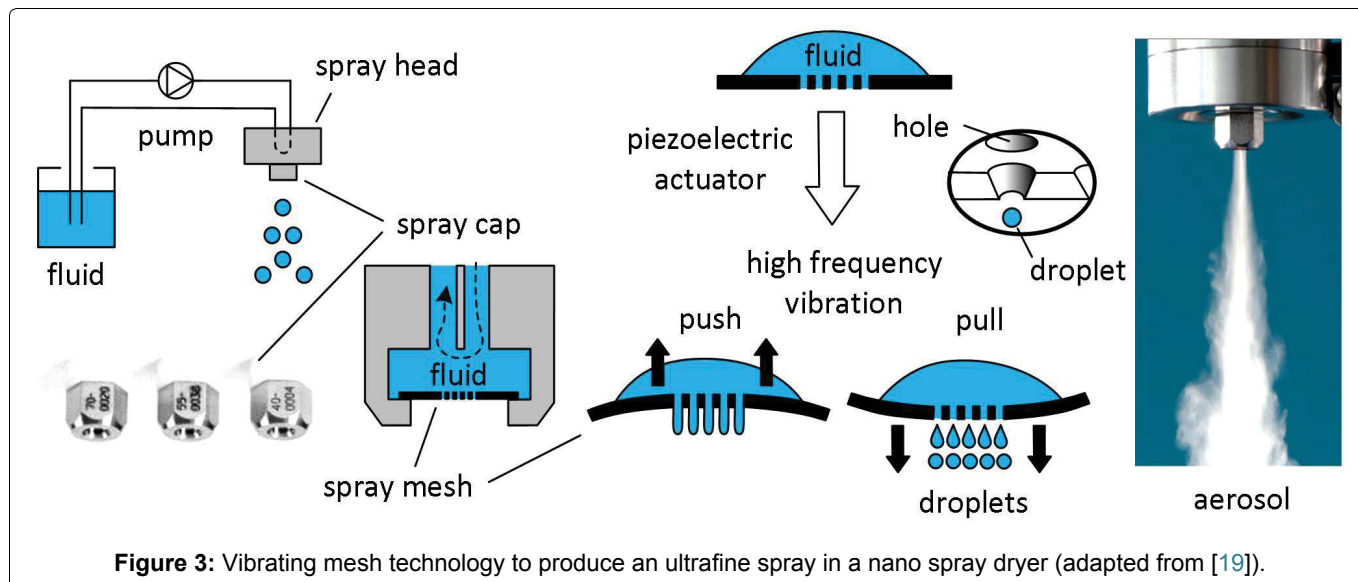
[10,14,23,25,26]. Nano spray drying enables the encapsulation of active ingredients in polymeric wall materials providing enhanced environmental protection (e.g. against oxidation, light, and temperature), stability, handling, storage, and controlled drug release properties. The nanonization and structural change improves the particle solubility and redispersibility of the final drug product in aqueous solutions.

This study explains the concept of nano spray drying, the influence of the main process parameters on the powder properties (e.g. particle size, morphology, encapsulation efficiency, drug loading), and discusses different pharmaceutical applications realized in the laboratory-scale.

Process Parameters of a Nano Spray Dryer

Figure 2 shows a schematic representation and the functional principle of a nano spray dryer. The adjustable process parameters (e.g. drying gas flow rate, inlet temperature, and spray rate) and formulation variables (e.g. feed composition, solid concentration) are colored in black. The resulting parameters like the





drying gas outlet temperature, the droplet and dried particle size, the product yield, and others are marked in grey. Overall, nano spray drying offers flexibility for formulation and a whole range of process parameters influence the final spray dried particle properties.

The droplet generation is based on vibrating mesh technology, which has been adapted from nebulizers used in aerosol drug delivery (Figure 3). A piezoelectric actuator vibrates a small replaceable spray cap at ultrasonic frequency. The cap comprises a thin perforated metal mesh containing a series of tiny laser drilled holes. Figure 3 illustrates a typical hole in the mesh. The piezoelectric vibration leads to a fast upward and downward movement of the spray mesh, thus ejecting millions of precisely sized droplets through the holes into the drying chamber. The droplet size depends on the mesh size and the physicochemical properties of the fluid, such as viscosity and surface tension. Spray meshes are available with 4.0, 5.5, and 7.0 μm hole diameters [19]. With a 4.0 μm spray mesh approximately 3 to 8 μm water droplets are produced [12,19,27].

The co-current drying gas flow is heated up to the set inlet temperature and directs the particles to the

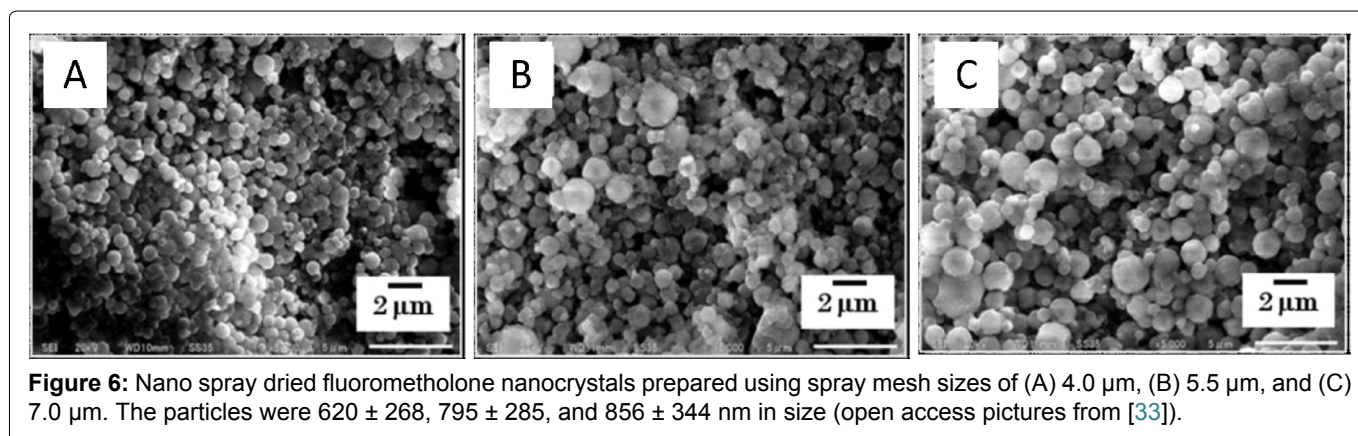
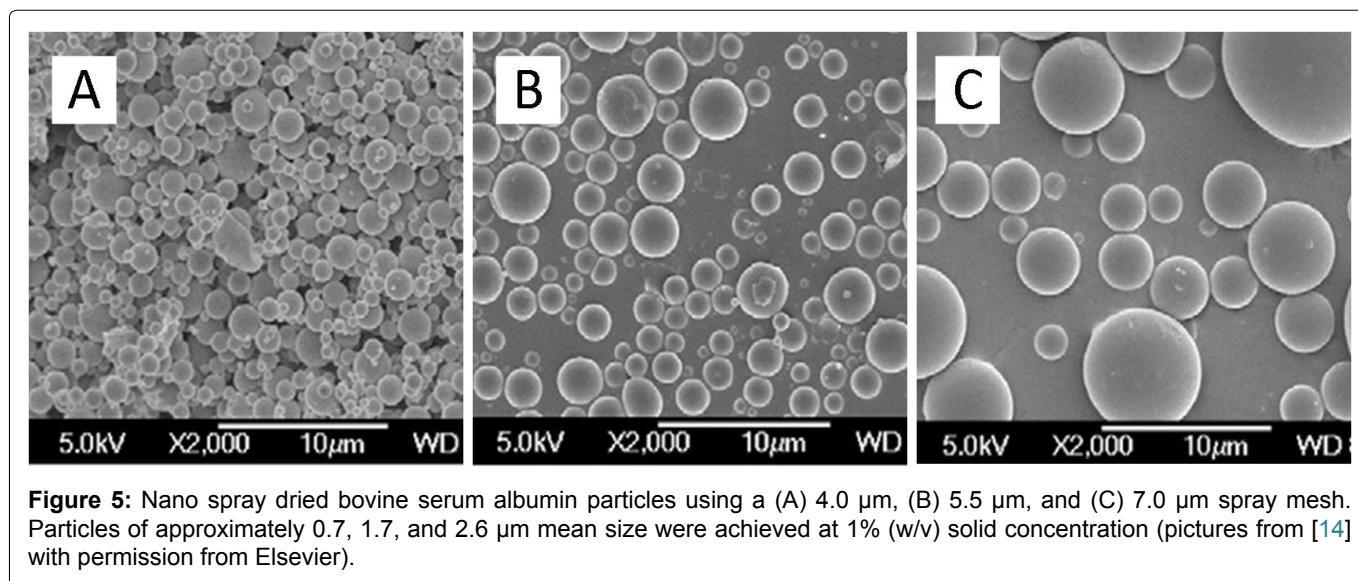
electrostatic particle collector. The dried particles are electrostatically charged and captured at high efficiency [14,20]. The flow of the drying gas is laminar, which makes the system suitable for gentle drying heat-sensitive products with a low risk of degradation or loss of activity. The drying gas exits the spray dryer in a purified form and the outlet temperature is measured.

The electrostatic particle collector can capture submicron particles ($< 1 \mu\text{m}$) at a separation efficiency greater than 99% for small solid batches of 30 to 500 mg [10,12,14,15] (Figure 4). The electrostatic precipitator can even collect thin-walled particles without breaking [29,30]. The particles are gently removed from the internal surface of the collecting electrode cylinder by utilizing the particle scraper and particle collecting paper that are included in the delivery of the laboratory instrument. Uniquely high yields of 76 to 96% are obtained, thus enabling the economical use of expensive pharmaceutical ingredients and pure drugs.

During spray drying, the cooling effect of the evaporating solvent keeps the droplet temperature low, so that heat sensitive products like proteins, peptides, hormones, or amino acids can be stabilized

Table 2: Influence of the main process parameters in nano spray drying (▲/▼ strong, ↑/↓ weak increasing/decreasing influence, - minimal or no influence) (adapted from [19]).

Process parameter	Outlet temperature	Droplet size	Particle size	Feed rate	Moisture content	Yield	Stability
Drying gas flow rate ↑	▲	-	-	-	▼	-	-
Drying gas humidity ↑	↑	-	-	-	▲	↓	-
Inlet temperature ↑	▲	-	↑	-	↓	↑	▼
Spray mesh size ↑	↓	▲	▲	▲	-	-	↑
Spray rate intensity ↑	▼	↑	↑	▲	↑	-	▼
Circulation pump rate ↑	-	↑	↑	↑	-	-	↑
Solid concentration ↑	↑	-	▲	▼	↓	↑	-
Surfactant/stabilizer ↑	-	↓	↓	↑	-	-	▲
Solvent instead of water	▲	↓	↓	↑	▼	↑	-



in nanopowder forms at optimized product yields and dried with negligible degradation.

Table 2 gives an overview of the main process parameters and their influence on the output parameters (i.e. outlet temperature, droplet size, feed rate) and the final product properties (i.e. particle size, moisture content, yield, stability). The thickness of each arrow illustrates the strength of the related influence. The key parameters controlling the final particle size are the spray mesh size and the solid concentration. The submicron size is typically reached when a 4.0 μm spray mesh and diluted solutions of 0.1 to 1% (w/v) are used.

Several authors investigated the relationship between spray mesh aperture size and particle size of drugs. The spray mesh size determines directly the size of the droplets and consequently the dried solid particles. As examples, Figure 5 and Figure 6 shows some SEM images of the model protein bovine serum albumin and the asthma drug fluorometholone obtained with a 4.0, 5.5, and 7.0 μm spray mesh respectively. The average particle size decreased with decreasing mesh aperture size producing smaller droplet, for the fluorometholone particles 620 ± 268 , 795 ± 285 , and 856 ± 344 nm for mesh aperture sizes of 4.0, 5.5, and 7.0 μm, respectively. The bovine serum

Table 6: Typical first-guess experimental process parameters for nano spray drying of pharmaceuticals.

Solvent	Inlet drying temperature [°C]	Outlet drying temperature [°C]	Drying gas type	Drying gas flow rate [L/min]	Solid concentration [% w/v]	Spray mesh size [µm]	Feed Rate [mL/h]
Water	60 to 120	30 to 60	Air Air Inert gas (N ₂ /CO ₂)	100 to 140	0.1 to 10	4.0 5.5 7.0	5 to 25 20 to 65 30 to 160
Ethanol	50 to 110	30 to 50		100 to 120			
Acetone	40 to 70	25 to 40		90 to 120			
DCM	30 to 50	20 to 35		80 to 120			

albumin particles were approximately 0.7, 1.7, and 2.6 µm in size respectively at 1% (w/v) solid concentration.

The validity of these results is supported by various reports [14,17,19,31]. It should be noted here that at an ultrasonic vibration frequency of 100 kHz and assuming 100 active holes per spray mesh, a fine mist of around 10 million droplets per second is produced.

Table 3 presents the particle sizes that have been realized by nano spray drying for various pharmaceutical applications. The key parameters controlling the final particle size are the spray mesh size [14,31,32] and the solid concentration [10-12,14,27]. Smaller droplets are favored by a higher viscosity, a lower surface tension, and a smaller spray mesh [14,15,33-35]. The region of submicron particle size is typically reached when using a 4.0 µm spray mesh and diluted solutions of 0.1 to 1% (w/v). Further reduction of particle size is possible by further dilution, as demonstrated in several studies [10,14,31,33,36-39].

Depending on the application, an optimized set of process parameters can be found, e.g. by design of experiment studies, as shown by several authors [10,15,16,19]. The selection of the organic solvent is based on the drug solubility and the encapsulating wall materials, as well as on the required drying temperatures. For aqueous applications, the outlet temperatures range between 28 and 59 °C [20]. The optimal drying temperatures of for example poly(lactic-co-glycolic acid) (PLGA) dissolved in dichloromethane lies in a range of 29 to 32 °C [16].

Typical organic solvents applied in nano spray drying of pharmaceuticals are:

- dichloromethane (DCM) [16,33,40-44],
- acetone [10,44-50],
- ethanol [15,31,32,51,52],
- methanol [27,53-56],
- acetonitrile [57,58],
- ethyl acetate [44], and
- mixtures thereof with water [59-65].

The selection of the organic solvent is based on the solubility of the drug and the encapsulating wall materials (e.g. excipients). The mixing ratio is adjusted to allow the complete dissolution of the compounds [61].

For example, acetone-water mixtures dissolve steroidal dexamethasone well, and the low viscosity of the acetone allows higher flow rates through the vibrating spray mesh, which shortens the processing time [48]. Compared to water, organic solvents generate slightly smaller droplets due to their lower surface tension, viscosity, and density [54]. In addition, organic solvents enable lower drying temperatures because of the lower boiling points. Dichloromethane (40 °C) or acetone (56 °C) lead to fast drying and prevent particles from sticking to the walls or agglomerating. The evaporation temperature is lower than the melting temperature or the glass transition temperature of certain polymers (Table 3).

Numerous excipients, dispersing agents, binders and stabilizers are applied in drug formulation studies, including:

- water-soluble saccharides (e.g. Arabic gum, alginate, chitosan, cyclodextrin, cellulose derivatives, modified starch, maltodextrin, pectin, mannitol, lactose trehalose),
- proteins (i.e. gelatin, serum albumin, whey protein, sodium caseinate, silk fibroin, leucine),
- water-soluble synthetic polymers (e.g. poly(vinyl alcohol), poly(ethylene glycol) or poly(acrylic acid) (Carbopol)),
- hydrophobic synthetic polymers (e.g. PLGA, poly(ε-caprolactone), poly(vinyl pyrrolidone) (Kollidon), Eudragit), and
- fats (e.g. stearic acid and glyceryl behenate (Compritol)).

The selection of a suitable matrix excipient is essential for the encapsulation of drugs by nano spray drying to achieve the desired decomposition of the particles and the drug release in the lungs.

- Mannitol, chitosan, leucine, lactose, and trehalose are widely used due to their high aqueous solubility and low toxicity.
- The hygroscopic excipient mannitol is especially advantageous for the treatment of bacterial infections in cystic fibrosis [70,71].
- Chitosan offers several advantages for mucosal delivery, such as low toxicity and good biodegradability as well as antibacterial activity [36,62,68,72-74].

Table 3: Influence of spray mesh size on final nano spray dried particle size in nm (n.a. = data not available).

Substance	Solvent	Concentration (% w/v)	Mesh size			Reference
			4.0 μm	5.5 μm	7.0 μm	
Chitosan (low-density)	0.5% acetic acid	0.025	95	215	265	[36]
Ethambutol	Water	1	220	n.a.	n.a.	[66]
Gentamicin sulfate in alginate/pectin	Water	0.1	310	520	850	[34]
		0.25	345	550	980	
		0.5	405	610	1,000	
Arabic gum	Water	0.1	355	n.a.	n.a.	[10]
		1	580	n.a.	n.a.	
Whey protein	Water	0.1	420	n.a.	n.a.	[10]
		1	595	n.a.	n.a.	
Sodium chloride	Water	0.1	515	n.a.	n.a.	[10]
		1	995	n.a.	n.a.	
Disodium phosphate	Water	0.1	500	n.a.	n.a.	[12]
Trehalose	Water	0.1	800	n.a.	n.a.	[12]
Bovine serum albumin (with surfactant)	Water	0.1	460	n.a.	n.a.	[14]
		1	700	1,700	2,600	
Sodium alginate	Water	0.13	760	n.a.	n.a.	[67]
Vancomycin in chitosan	0.5% acetic acid	0.2	450	n.a.	n.a.	[68]
Curcumin in albumin	Water	0.5	715	n.a.	n.a.	[69]
Salbutamol sulfate	Water	1	1,000	1,600	3,100	[35]
Galactosidase in trehalose	Water	5	1,800	4,500	4,900	[15]
CsH ₂ PO ₄	Methanol:water (56:44)	0.1	200	300	500	[54]
		1	540	n.a.	n.a.	
Calpain inhibitor steroid nanocrystals	Ethanol	0.05	420	605	845	[32]
		0.5	995	n.a.	n.a.	
Fluorometholone	Ethanol	0.1	620	795	855	[31]
Dexamethasone	Ethanol	1	835	1,100	1,300	[31]
PLGA	DCM	1	n.a.	3,200	4,200	[43]
Ethyl cellulose	DCM	1	1,500	2,700	3,400	[42]
PLGA	DCM	0.5	n.a.	570	n.a.	[33]
		1	n.a.	760	n.a.	
		2	685	830	930	
		5	n.a.	1,100	n.a.	

- Leucine is a very popular dispersion enhancer to increase the flowability of nano spray dried particles, as shown in various pulmonary drug delivery studies [30,59-62,64,73,75-82].

Table 4 summarizes typical process parameters of various wall materials (excipients) used as dispersants, binders and stabilizers in the nano spray drying of pharmaceuticals at laboratory-scale.

The morphology of particles prepared by nano spray drying depends on the drying conditions and the feed properties. Dense, hollow, porous, composites, and encapsulated structures (i.e. single-core, multi-core, irregular, or multi-walled) with spherical, wrinkled, shriveled, or even doughnut-like shapes can be obtained [19]. Figure 7 illustrates some examples of nano spray dried particles including salbutamol, albuterol in mannitol, cyclosporine in PLGA, trehalose, β -galactosidase in trehalose, and bovine serum albumin.

In general, slow drying leads to more compact particles, while fast and high temperature drying favors the formation of hollow particles with thin shells. Surfactants

balance the surface-to-viscous forces inside of the drying droplet and enable the formation of a smooth spherical surface. Composite particles prepared from suspensions and nano spray drying provide a high specific surface area. Most nano spray dried drugs tend to be amorphous due to the too short drying time to form crystalline structures. To prevent recrystallization, the dried powders are stored under dry and controlled conditions.

Of primary interest for pharmaceuticals are the effects on the particle size, morphology, yield, productivity, encapsulation efficiency, drug loading, drug release profile, and stability.

Table 5 summarizes some representative literature data on encapsulation efficiency and drug exposure. Particles with an encapsulation efficiency of over 95% and an adjustable drug load were produced. Further information on yield and optimized process parameters of nano spray drying are given.

Applications of Nano Spray Dried Pharmaceuticals on the Laboratory-Scale

The number of publications on nano spray dried

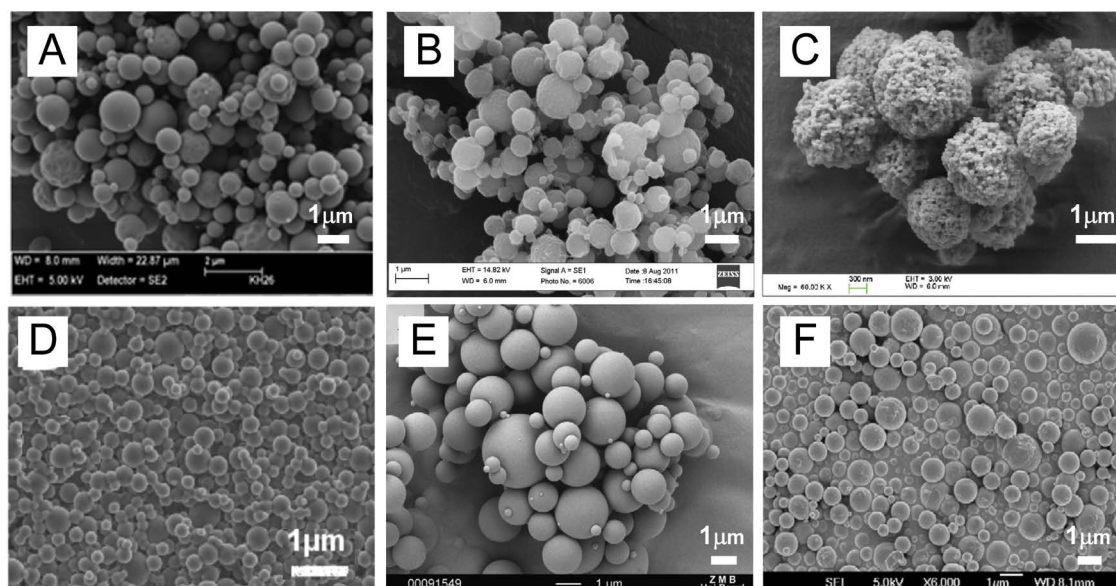


Figure 7: Examples of nano spray dried particles: A: Salbutamol sulfate (1% solid concentration, nano spray dried at 100 °C) [37]; B: Albuterol sulfate in mannitol, L-leucine and poloxamer 188 (30:48:20:2 mixing ratio, 0.5% in water-ethanol solution (80:20), 70 °C) [65]; C: Cyclosporin in PLGA (50:50, 15 kDa, dissolved in DCM, 29 °C) [16]; D: Trehalose with addition of 0.005% polysorbate 20 (0.1%, 120 °C) [12]; E: β -galactosidase in trehalose (1:2 mixing ratio, 5%, 80°C) [15]; F: Bovine serum albumin with 0.05% Tween 80 (0.5%, 120 °C) [14].

Table 4: Different wall materials applied for encapsulation of pharmaceuticals by nano spray drying (n.a. = not available).

Encapsulation wall materials (excipient)	Solvent	T in (°C)	T out (°C)	Drying gas (L/min)	Particle size (μ m)	Solid sample amount (mg)	Product yield (%)	References
Arabic gum, whey protein, maltodextrin, polyvinyl alcohol and modified starch	Water	100	38 to 60	100	0.2 to 1.1	30 to 300	43 to 95	[10]
Sodium alginate (polysaccharide)	Water	110	n.a.	100	0.4 to 1.2	n.a.	> 90	[67]
Trehalose, mannitol or disodium phosphate surfactant, polysorbate	Water	60 to 100	30 to 45	115	0.3 to 3	10 to 50	50 to 78	[11,12,27]
Leucine (amino acid, dispersing agent), Trehalose (stabilizer, increases shelf life)	Water	75	45	100	2.1 to 5.4	n.a.	n.a.	[29]
Nanosuspension of mannitol and poly(lactic-co-glycolic acid) (PLGA)	Water	80	32 to 39	140	1.1 to 7.2	n.a.	n.a.	[70]
Chitosan (biopolymer, fat blocker)	Water, Acetic acid	120	55	130	0.6 to 1.6	n.a.	n.a.	[83]
PLGA (biodegradable polymer)	Dichloromethane (DCM)	30 to 50	20 to 30	100	2.8 to 4.4	n.a.	n.a.	[33]
PLGA suspensions	DCM	30 to 50	20 to 30	100	0.3 to 1.7	n.a.	n.a.	[33]
PLGA (fine carrier supports)	DCM	n.a.	n.a.	100 (N ₂ /CO ₂)	1 to 16	n.a.	n.a.	[84]
PLGA and stabilizers (poloxamer, surfactant)	Acetone, Ethyl acetate, DCM,	50 to 90	29 to 36	115 (N ₂ /CO ₂)	2.4 to 8	1'080 to 1'350	60 to 85	[44]
Hypromellose (hydroxypropyl-methylcellulose, for oral medicaments)	Acetone	36 - 68	n.a.	90 to 120	2 to 10	800	75 to 91	[50]

pharmaceuticals on the laboratory-scale has risen sharply after the market launch of the Nano Spray Dryer B-90 in 2009 [19]. The formulations contain drugs and excipients for the treatment of various diseases, including:

- *asthma* (e.g. salbutamol, terbutaline, or fluticasone) [31,35,51,75-79,89,93-98],
- *inflammation* (e.g. dexamethasone and azithromycin, or pain and fever reducer indomethacin and nimesulide) [16,31,45,47,48,53,55,64,71,99-101],
- *cystic fibrosis* (e.g. antibacterial dexketoprofen in Kollidon and Eudragit nanoparticles, or azithromycin in leucine) [64,70,71],
- *diabetes* (e.g. sitagliptin, vildagliptin, and metformin in mucoadhesive Carbopol and gelatin) [102-104],
- *pulmonary arterial hypertension* (e.g. resveratrol in poly(caprolactone), or sildenafil in PLGA) [39,86],
- *tuberculosis* (e.g. capreomycin or pyrazinamide in L-leucine, or ethambutol mixed with chitosan carrier particles) [59-61,66,81,82]
- *Alzheimer's and Parkinson's diseases* (e.g. nanocrystals of calpain inhibitor steroids) [32,88],
- *breast cancer* (e.g. simvastatin loaded PLGA particles), or lung cancer (e.g. methotrexate, carboplatin in gelatine, or paclitaxel) [90,91,105-108],
- *bacterial infections* (e.g. amoxicillin, ciprofloxacin, gatifloxacin, clarithromycin, or levofloxacin),
- *fungal infections* (e.g. antifungal griseofulvin) [27,52],
- *ophthalmic disorders* (e.g. calpain inhibitor nanocrystals or dirithromycin incorporated in Kollidon) [31,32,56],
- *high blood pressure* (e.g. nimodipine in PLGA or pure nicergoline nanoparticles) [41,65],
- *congestive heart failure* [86] and edema (e.g. diuretic furosemide) [10].

The number of applications reviewed in this study underlines the versatility of the nano spray drying technology to develop nanomedicines. As illustrated in Figure 4 the drug-loaded nano spray dried powders are administered through various ways, such as:

- *pulmonary* (e.g. optimized respirable particles of 1 to 5 μm size),
- *oral* (e.g. poorly water-soluble drugs like diuretic furosemide [10], pain reducing nimesulide [100], blood vessels dilating nicergoline [67], fever reducing indomethacin [99], anti-inflammatory dexamethasone [46], or steroidal hormone mecigestone [109]),
- *intravenous* (e.g. simvastatin in PLGA as cancer chemotherapeutics, antipsychotic clozapine and risperidone in PLGA, or small interfering RNAs loaded

in human serum albumin particles to treat genetic disorders),

- *topically* as creams to the skin (e.g. anti-inflammatory dexamethasone, antibacterial gentamicin in gelatin-pectin, amoxicillin loaded chitosan, antifungal econazole in cyclodextrin, soy isoflavones for skin cancer treatment or as anti-ageing agent), or as nanoparticulate powder (e.g. as a wound dressing during surgery),
- *ophthalmic* (e.g. anti-inflammatory steroids in eye drop solutions, or dirithromycin to treat ocular bacterial infections),
- *intraperitoneal* (e.g. encapsulated paclitaxel as cytostatic in anticancer therapy),
- *intravesical* (e.g. as drug delivery system to treat local bladder diseases), and even
- *cerebral* (e.g. with nimodipine in PLGA regulating the dilatation of blood vessels).

The nano spray drying process is gentle and contributes to maintaining the stability and activity of heat-sensitive materials, such as peptides, proteins, hormones and amino acids. This has been confirmed for example by nano spray drying bacitracin (polypeptide antibiotic) [82] or insulin-like growth factor I (anabolic peptide) encapsulated in trehalose, silk fibroin and polysorbate [86] (see Table 4).

To sum up, Table 6 lists typical experimental process parameters for nano spray drying that can be used as first guess values for applying identical or similar substances. The main organic solvents used to dissolve poorly water-soluble drugs are ethanol, acetone, and DCM. With highly diluted solutions containing 0.1 to 1% (w/v) solids concentrations, finest solid particles down to 100 nm can be obtained by nano spray drying.

Pure drug particles in the nanosize dimensions and the amorphous state offer higher absorption rates and bioavailability and encourage future developments in this research area. Nanocapsules, with their reduced size and large specific surface area, provide pronounced improvement in controlled drug release and bioavailability. This enables the generation of target drug delivery systems. Under optimized conditions, uniquely high product yields of about 76 to 96% can be achieved to process small sample amounts of substances in the range of 10 mg to 2.5 g.

Variations in the yield may occur due to particle depositions around the spray cap and the chamber walls, nozzle blockage, or due to losses during the manual collection of the powder with a rubber spatula (Figure 8).

However, the ability to process small sample amounts makes a nano spray dryer very suitable for testing valuable biological materials such as for example

Table 5: Published studies on nano spray dried drug delivery applications structured by administration routes (Drug loading (%) = Amount of drug in particles/Total mass of particles, Encapsulation efficiency (%) = Amount of drug in particles/Initial drug amount, n.a. = not available).

Drug substance, Encapsulation wall material (excipient), Application	Solvent	T in (°C)	T out (°C)	Drying gas (L/min)	Particle size (µm)	Solid sample amount (mg)	Product yield (%)	Drug loading (%)	Encapsulation efficiency (%)	References
Cyclosporin (Immune system suppressant)	DCM, Ethanol	29 to 32	28 to 32	102 to 132 (N ₂ /CO ₂)	0.9 to 2.2	600	20 to 56	13 to 14	38 to 41	[16]
Dexamethasone (Steroid, anti-inflammatory)	DCM, Ethanol	29 to 30	30 to 32	111 to 132 (N ₂ /CO ₂)	0.9 to 1.7	600	32 to 54	21 to 27	62 to 81	[16]
Dexamethasone (Steroid, anti-inflammatory)	Acetone Water	55	34	110	0.6 to 1.6	210	65 to 80	43	93 to 97	[48]
Insulin-like growth factor I (Anabolic peptide)	Water	70	n.a.	115 to 130	0.3 to 3.2	n.a.	n.a.	74	93	[85]
Resveratrol (Pulmonary arterial hypertension)	Acetone, Water	55	n.a.	110 (N ₂ /CO ₂)	1.0 to 5.0	300	71 to 88	31	99	[86]
Acyclovir (Antiviral and antiherpetic agent)	Water, DCM	85	n.a.	n.a.	< 0.5	n.a.	75	22	85	[87]
Dextetropfen, Trometamol (Anti-inflammatory, analgesic delivery)	Methanol	120	54	n.a.	0.1 to 0.7	1'000	n.a.	n.a.	36 to 51	[53,55]
Selegiline (Parkinson's disease, depression)	Water	120	27	100 to 110	0.1 to 0.2	n.a.	86 to 93	98	97 to 99	[88]
Vancomycin (Antibiotic, colon drug delivery)	Water	80	40	n.a.	0.4 to 0.5	400	74 to 88	52 to 64	68 to 76	[68]
Clozapine and risperidone (Antipsychotic drugs to treat Schizophrenia)	DCM Water	60 to 80	31 to 38	112 to 118 (N ₂)	0.2 to 0.4	100	48 to 64	6 to 13	89 to 98	[40]
Salbutamol sulphate (Asthma, targeting lungs passively after intravenous injection)	Water	80 to 120	20	90 to 95	1.2 to 10	n.a.	86	n.a.	72	[89]
Simvastatin (Breast cancer)	DCM, Water	n.a.	n.a.	n.a.	0.1 to 0.7	115	n.a.	9	63	[90]
Dexamethasone (Anti-inflammatory drug to treat skin diseases)	Acetone Water	55	n.a.	110	0.4 to 2.3	100	72 to 90	47	94	[47]
Gentamicin sulfate (Antibacterial drug for wound dressing)	Water	90	n.a.	100	0.3 to 1.0	n.a.	65 to 91	23 to 28	70 to 83	[34]

Soy bean isoflavones (Skin cancer treatment, anti-ageing agent, chemopreventive)	Hypromellose acetate succinate	Water, Ethanol	60	29	100	0.3 to 1.3	n.a.	60 - 88	n.a.	62 to 86	[91]
Soy bean isoflavone extract	CMC	Water	n.a.	n.a.	n.a.	~ 0.65	n.a.	n.a.	n.a.	78 to 89	[92]
Dirithromycin (Ocular bacterial infections)	Kollidon SR (Polyvinyl alcohol and polyvinylpyrrolidone)	Methanol	90	30 to 40	n.a.	0.3 to 0.5	n.a.	n.a.	n.a.	25 to 44	[56]
Thiolated glycol chitosan conjugates (Mucoadhesive, local bladder diseases)	N-acetylcysteine, Glutathione, Glycol, Chitosan	Water, Acetonitrile	40	30 to 32	100 (N ₂ /CO ₂)	0.2 to 1.4	n.a.	15 to 25	36 to 73	64 to 100	[58]
Nimodipine (Dilatation regulator in brain arterioles)	PLGA	DCM	45	n.a.	120	0.7 to 3.7	n.a.	n.a.	10 to 40	93 to 98	[41]

monoclonal antibodies, recombinant proteins, or siRNA-based therapeutics. Moreover, nano spray drying enables the encapsulation of drugs in polymers with high efficiency of over 95% and adjustable drug loading.

Conclusions

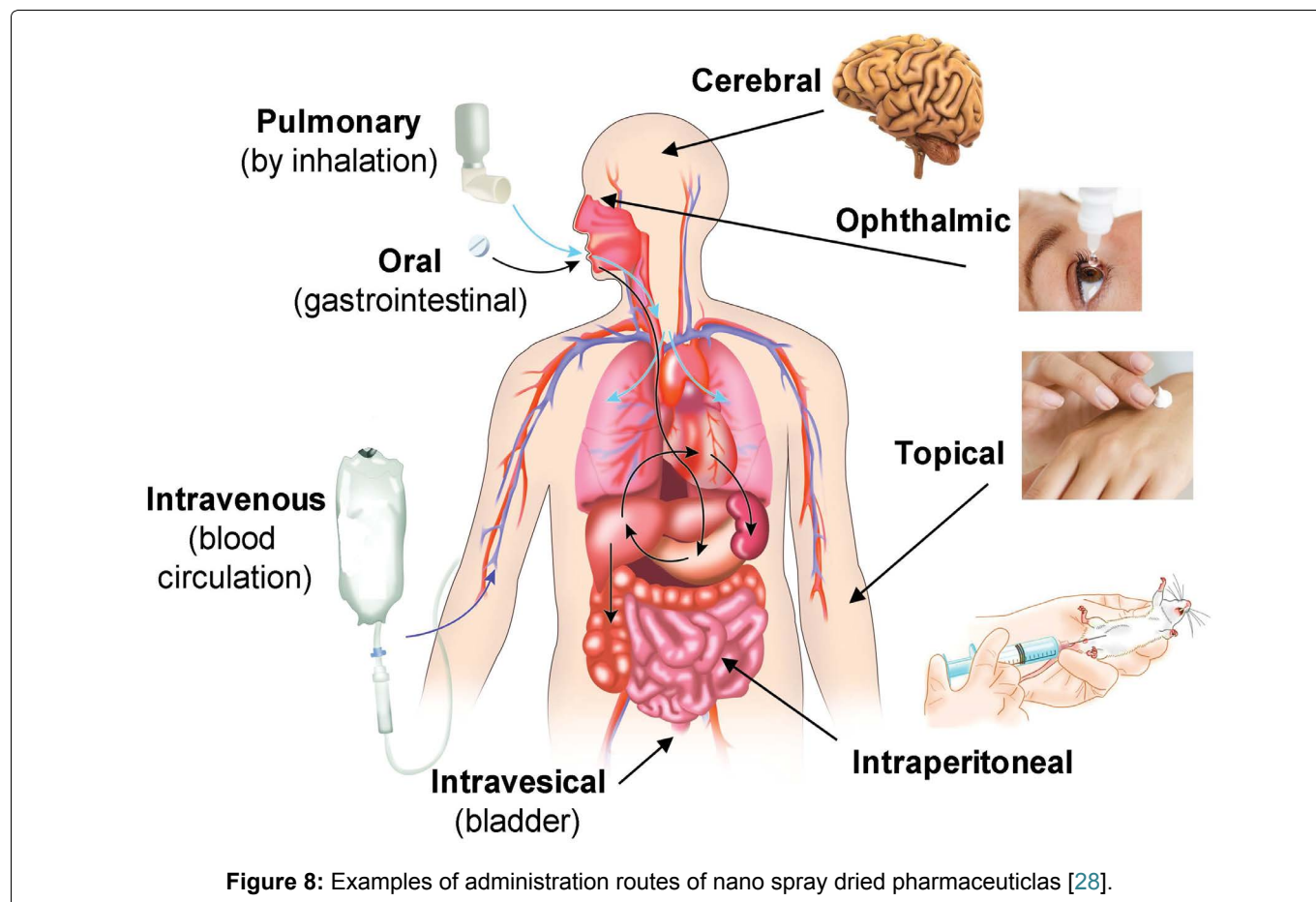
Nano spray drying has been successfully applied for a wide range of pharmaceutical applications on a laboratory-scale, such as increasing the bioavailability of poorly soluble drugs by nanoisation and structural modification, as well as the encapsulation of nanoparticles, nanoemulsions and nanosuspensions in biocompatible polymeric wall materials for sustained drug release. Encapsulation efficiencies of over 95% are achieved by adjustable drug loadings. Smallest sample amounts ranging from 10 mg to 2.5 g with uniquely high yields of over 95% can be processed, which enables the economical use of valuable active pharmaceutical ingredients.

Compared to conventional spray drying processes, nano spray drying relies on vibrating mesh technology to produce an ultrafine spray. A highly efficient electrostatic powder collector to extend the size spectrum of separable particles to the nanoscale.

The most important adjustable process parameters are the drying gas temperature, the drying gas flow rate, the spray mesh size, the solvent type, the solids concentration in the feed, and the selection of the corresponding excipients, stabilizers and surfactants. Depending on the application, an optimized set of parameters can be found. Submicron spray dried particles can be formed down to a size of only 100 nm with diluted solutions of 0.1 to 1% (w/v) solids concentration. Different particle morphologies can be created, including dense, hollow and porous particles with spherical, wrinkled, or donut shapes.

The drying process is gentle and contributes to maintaining the stability and activity of heat-sensitive materials, such as peptides, proteins, hormones and amino acids. The prepared drug loaded particles are administered in various ways, including pulmonary, oral, intravenous, topically, ophthalmic, intraperitoneal, intravesical, or even cerebral, which underlines the versatility of the nano spray drying technology.

With the introduction of the Nano Spray Dryer B-90 from Büchi Labortechnik AG (Switzerland) in 2009, the nano spray drying of protein nanotherapeutics became reality on a laboratory-scale [14]. It is expected that the increased customer demand for the laboratory product, combined with promising new applications, will promote and stimulate the development of more industry-relevant models [13]. In order to further explore the potential of nano spray drying, future research should focus on further commercialization of this technology on a pilot and industrial scale. The demand for larger quantities of powder and for the scale-up of nano spray



drying technology is increasing. To achieve this, however, equipment designed for a larger scale is required. A possible scale-up solution for droplet formation and throughput increase are several vibrating mesh atomizers in parallel arrangement (e.g. like ultrasonic humidifiers) or a larger nozzle unit. Industrial-scale electrostatic particle collectors with mechanical rapping devices can be installed for the collection of nanoparticles with an automatic cleaning system to continuously remove the separated particles from the collecting.

The main application trends in nano spray drying are seen in the areas of pulmonary drug delivery, nanotherapeutics, the encapsulation of nanoemulsions with poorly water-soluble active ingredients and the formulation of nanocrystals for a higher bioavailability.

References

- Broadhead J, Edmond Rouan SK, Rhodes CT (1992) The spray drying of pharmaceuticals. *Drug Dev Ind Pharm* 18: 1169-1206.
- Kawabata Y, Wada K, Nakatani M, Yamada S, Onoue S (2011) Formulation design for poorly water-soluble drugs based on biopharmaceutics classification system: Basic approaches and practical applications. *Int J Pharm* 420: 1-10.
- Huang Y, Dai WG (2014) Fundamental aspects of solid dispersion technology for poorly soluble drugs. *Acta Pharm Sin B* 4: 18-25.
- Brough C, Williams RO 3rd (2013) Amorphous solid dispersions and nano-crystal technologies for poorly water-soluble drug delivery. *Int J Pharm* 453: 157-166.
- Lam J, Vaughan S, Parkins MD (2013) Parkins, Tobramycin Inhalation Powder (TIP): An Efficient Treatment Strategy for the Management of Chronic *Pseudomonas Aeruginosa* Infection in Cystic Fibrosis. *Clin Med Insights Circ Respir Pulm Med* 7: 61-77.
- Konstan MW, Geller DE, Minić P, Brockhaus F, Zhang J, et al. (2011) Tobramycin inhalation powder for *P. aeruginosa* infection in cystic fibrosis: The EVOLVE trial. *Pediatr Pulmonol* 46: 230-238.
- Anderson SD, Daviskas E, Brannan JD, Chan HK (2018) Repurposing excipients as active inhalation agents: The mannitol story. *Adv Drug Deliv Rev* 133: 45-56.
- Guntur VP, Dhand R (2007) Inhaled Insulin: Extending the Horizons of Inhalation therapy. *Respir Care* 52: 911-922.
- Vehring R (2008) Pharmaceutical particle engineering via spray drying. *Pharm Res* 25: 999-1022.
- Li X, Anton N, Arpagaus C, Belleiteix F, Vandamme TF (2010) Nanoparticles by spray drying using innovative new technology: The Büchi Nano Spray Dryer B-90. *J Control Release* 147: 304-310.
- Schmid C, Arpagaus, Friess W (2009) Evaluation of a Vibrating Mesh Spray Dryer for Preparation of Submicron Particles. *Respir Drug Deliv* 323-326.
- Schmid K, Arpagaus C, Friess W (2011) Evaluation of the Nano Spray Dryer B-90 for pharmaceutical applications. *Pharm Dev Technol* 16: 287-294.
- Heng D, Lee SH, Ng WK, Tan RB (2011) The Nano Spray Dryer B-90 *Expert Opin Drug Deliv* 8: 965-972.
- Lee SH, Heng D, Ng WK, Chan HK, Tan RB (2011) Nano spray drying: A novel method for preparing protein nanoparticles for protein therapy. *Int J Pharm* 403: 192-200.

15. Bürki K, Jeon I, Arpagaus C, Betz G (2011) New insights into respirable protein powder preparation using a nano spray dryer. *Int J Pharm* 408: 248-256.
16. Schafroth N, Arpagaus C, Jadhav UY, Makne S, Douroumis D (2012) Nano and microparticle engineering of water insoluble drugs using a novel spray-drying process. *Colloids Surfaces B Biointerfaces* 90: 8-15.
17. Arpagaus C, Collenberg A, Rütli D, Assadpour E, Jafari SM (2018) Nano spray drying for encapsulation of pharmaceuticals *Int J Pharm* 546: 194-214.
18. Arpagaus C, Bless F, Uhlmann M, Schiffmann J, Bertsch SS (2018) High temperature heat pumps: Market overview, state of the art, research status, refrigerants, and application potentials. *Energy* 152: 985-1010.
19. Arpagaus C, John P, Collenberg A, Rütli D (2017) Chapter 10: Nanocapsules formation by nano spray drying. In: Jafari SM, Nanoencapsulation technologies for the food and nutraceutical industries. Elsevier Inc., 346-401.
20. Arpagaus C (2012) A Novel Laboratory-Scale Spray Dryer to Produce Nanoparticles. *Dry Technol* 30: 1113-1121.
21. Arpagaus C (2011) Nano Spray Dryer B-90: Literature review and applications.
22. Arpagaus C, Rütli D, Meuri M (2013) Chapter 18: Enhanced Solubility of Poorly Soluble Drugs Via Spray Drying. In: Douroumis D, Fahr A, Drug Delivery Strategies for Poorly Water-Soluble Drugs. John Wiley & Sons, Ltd., 551-585.
23. Wong TW, John P (2015) Advances in Spray Drying Technology for Nanoparticle Formation. In: May M, Aliofkhaezai, Handbook of Nanoparticles, no. Springer International Publishing, 1-16.
24. Arpagaus C (2010) Spray Drying R&D Solutions - BÜCHI's Nano Spray Dryer: A world novelty in laboratory scale. *ONdrugDelivery* 40-41.
25. Wui WT (2015) Nanospray Drying Technology: Existing Limitations and Future Challenges. *Recent Pat Drug Deliv Formul* 9: 185-186.
26. Kaialy W, Al Shafiee M (2016) Recent advances in the engineering of nanosized active pharmaceutical ingredients: Promises and challenges. *Adv Colloid Interface Sci* 228: 71-91.
27. Schmid K (2011) Spray drying of protein precipitates and Evaluation of the Nano Spray Dryer B-90. PhD Thesis, Ludwig-Maximilians-University, Munich.
28. Arpagaus C (2018) Nano Spray Drying of Pharmaceuticals," in IDS'2018 - 21st International Drying Symposium, Valencia, Spain, 1-8.
29. Feng AL, Boraey MA, Gwin MA, Finlay PR, Kuehl PJ, et al. (2011) Mechanistic models facilitate efficient development of leucine containing microparticles for pulmonary drug delivery. *Int J Pharm* 409: 156-163.
30. Sun Y, Song X, Wang J, Yu J (2011) Preparation of lithium carbonate hollow spheres by spray pyrolysis. *Cryst Res Technol* 46: 173-177.
31. Baba K, Nishida K (2013) Steroid Nanocrystals Prepared Using the Nano Spray Dryer B-90. *Pharmaceutics* 5: 107-114.
32. Baba K, Nishida K (2012) Calpain inhibitor nanocrystals prepared using Nano Spray Dryer B-90. *Nanoscale Res Lett* 7: 1-9.
33. Beck-Broichsitter M, Schweiger C, Schmehl T, Gessler T, Seeger W, et al. (2012) Characterization of novel spray-dried polymeric particles for controlled pulmonary drug delivery. *J Control Release* 158: 329-335.
34. De Cicco F, Porta A, Sansone F, Aquino RP, Del Gaudio P (2014) Nanospray technology for an in situ gelling nanoparticulate powder as a wound dressing. *Int J Pharm* 473: 30-37.
35. Litringer Em, Zellnitz S, Hammernik K, Adamer V, Friedl H, et al. (2013) Spray Drying of Aqueous Salbutamol Sulfate Solutions Using the Nano Spray Dryer B-90 - The Impact of Process Parameters on Particle Size. *Dry Technol* 31: 1346-1353.
36. Kim LT, NganSan-Lang Wang, Minh Hiep D, Luong PM, Vui NT, et al. (2014) Preparation of chitosan nanoparticles by spray drying, and their antibacterial activity. *Res Chem Intermed* 40: 2165-2175.
37. Pérez-Masiá R, López-Nicolás R, Periago MJ, Ros G, Lagaron JM, et al. (2015) Encapsulation of folic acid in food hydrocolloids through nanospray drying and electrospraying for nutraceutical applications. *Food Chem* 168: 124-133.
38. Nandiyanto ABD, Okuyama K (2011) Progress in developing spray-drying methods for the production of controlled morphology particles: From the nanometer to submicrometer size ranges. *Adv Powder Technol* 22: 1-19.
39. Beck-Broichsitter M, Paulus IE, Greiner A, Kissel T (2015) Modified vibrating-mesh nozzles for advanced spray-drying applications. *Eur J Pharm Biopharm* 92: 96-101.
40. Panda A, Meena J, Katara R, Majumdar DK (2014) Formulation and characterization of clozapine and risperidone co-entrapped spray-dried PLGA nanoparticles. *Pharm Dev Technol* 21: 43-53.
41. Bege N, Renette T, Endres T, Beck-Broichsitter M, Hänggi D, et al. (2013) In situ forming nimodipine depot system based on microparticles for the treatment of posthemorrhagic cerebral vasospasm. *Eur J Pharm Biopharm* 84: 99-105.
42. Dahili LA, Kelemen-Horváth I, Feczko T (2015) 2,4-Dichlorophenol removal by purified horseradish peroxidase enzyme and crude extract from horseradish immobilized to nano spray dried ethyl cellulose particles. *Process Biochem* 50: 1835-1842.
43. Dahili LA, Feczko T (2015) Cross-linking of Horseradish Peroxidase Enzyme to Fine Particles Generated by Nano Spray Dryer B-90. *Period Polytech Chem Eng* 59: 209-214.
44. Draheim C, de Crécy F, Hansen S, Collnot EM, Lehr CM (2015) A Design of Experiment Study of Nanoprecipitation and Nano Spray Drying as Processes to Prepare PLGA Nano- and Microparticles with Defined Sizes and Size Distributions. *Pharm Res* 32: 2609-2624.
45. Durli TL, Dimer FA, Fontana MC, Pohlmann AR, Beck RC, et al. (2014) Innovative approach to produce submicron drug particles by vibrational atomization spray drying: influence of the type of solvent and surfactant. *Drug Dev Ind Pharm* 40: 1011-1020.
46. Perecin CJ (2015) Magnetite Nanoparticles Encapsulated with PCL and Poloxamer by Nano Spray Drying technique," in XIV Brazil MRS (Materials Research Society) Meeting, Rio.
47. Beber TC, Andrade DF, Kann B, Fontana MC, Coradini K, et al. (2014) Submicron polymeric particles prepared by vibrational spray-drying: Semisolid formulation and skin penetration/permeation studies. *Eur J Pharm Biopharm* 88: 602-613.
48. Fontana MC, Durli TL, Pohlmann AR, Guterres SS, Beck RCR (2014) Polymeric controlled release inhalable powder produced by vibrational spray-drying: One-step preparation and in vitro lung deposition. *Powder Technol* 258: 49-59.

49. Beck-Broichsitter M, Strehlow B, Kissel T (2015) Direct fractionation of spray-dried polymeric microparticles by inertial impaction. *Powder Technol* 286: 311-317.
50. Gu B, Linehan B, Tseng YC (2015) Optimization of the Büchi B-90 spray drying process using central composite design for preparation of solid dispersions. *Int J Pharm* 491: 208-217.
51. Zellnitz S, Narygina O, Resch C, Schroettner H, Urbanetz NA (2015) Crystallization speed of salbutamol as a function of relative humidity and temperature. *Int J Pharm* 489: 170-176.
52. Maged A, Mahmoud AA, Ghorab MM (2017) Hydroxypropyl-Beta-Cyclodextrin as Cryoprotectant in Nanoparticles Prepared by Nano-Spray Drying Technique. *J Pharm Sci Emerg Drugs* 5: 1-5.
53. Öztürk, Yenilmez E, Yazan Y (2015) Preparation and Characterization of Dexketoprofen Trometamol Loaded Kollidon-SR Nanoparticles," in ISOPS 11th International Symposium on Pharmaceutical Sciences, Ankara, Turkey,
54. Suryaprakash RC, Lohmann FP, Wagner M, Abel M, Varga A (2014) Spray drying as a novel and scalable fabrication method for nanostructured C₅H₂PO₄, Pt-thin-film composite electrodes for solid acid fuel cells. *RSC Adv* 4: 60429-60436.
55. Öztürk, Yenilmez E, Arslan R, Şenel B, Yazan Y (2017) Dexketoprofen Trometamol-Loaded Kollidon® SR and Eudragit® RS 100 Polymeric Nanoparticles: Formulation and In Vitro-In Vivo Evaluation. *Lat Am J Pharm Am J Pharm* 36: 2153-2165.
56. Basran E (2017) Ocular Application of Dirithromycin Incorporated Polymeric Nanoparticles: an In Vitro Evaluation. *Turkish J Pharm Sci* 14: 191-200.
57. Amsalem O, Nassar T, Benhamron S, Lazarovici P, Benita S, et al. (2017) Solid nano-in-nanoparticles for potential delivery of siRNA. *J Control Release* 257: 144-155.
58. Denora N, Lopodota A, Perrone M, Laquintana V, Iacobazzi RM, et al. (2016) Spray-dried mucoadhesives for intravesical drug delivery using N-acetylcysteine- and glutathione-glycol chitosan conjugates. *Acta Biomater* 43: 170-184.
59. Kaewjan K, Srichana T (2016) Nano spray-dried pyrazinamide-L-leucine dry powders, physical properties and feasibility used as dry powder aerosols. *Pharm Dev Technol* 21: 68-75.
60. Schoubben A, Blasi P, Giontella A, Giovagnoli S, Ricci M (2015) Powder, capsule and device: An imperative ménage à trois for respirable dry powders. *Int J Pharm* 494: 40-48.
61. Schoubben A, Blasi P, Marenzoni ML, Barberini L, Giovagnoli S, et al. (2013) Capreomycin supergenerics for pulmonary tuberculosis treatment: Preparation, in vitro, and in vivo characterization. *Eur J Pharm Biopharm* 83: 388-395.
62. Dimer F, de Souza Carvalho-Wodarz C, Hauptenthal J, Hartmann R, Lehr CM (2015) Lehr, Inhalable Clarithromycin Microparticles for Treatment of Respiratory Infections. *Pharm Res* 32: 3850-3861.
63. Son YJ, Longest PW, Tian G, Hindle M (2013) Evaluation and modification of commercial dry powder inhalers for the aerosolization of a submicrometer excipient enhanced growth (EEG) formulation. *Eur J Pharm Sci* 49: 390-399.
64. Aquino RP, Stigliani M, Del Gaudio P, Mencherini T, Sansone F, et al. (2014) Nanospray Drying as a Novel Technique for the Manufacturing of Inhalable NSAID Powders. *The Scientific World Journal*.
65. Martena V, Censi R, Hoti E, Malaj L, Martino PD (2012) A new nanospray drying method for the preparation of nicergoline pure nanoparticles. *J Nanoparticle Res* 14: 1-10.
66. Ahmad MI, Ungphaiboon S, Srichana T (2014) The development of dimple-shaped chitosan carrier for ethambutol dihydrochloride dry powder inhaler. *Drug Dev Ind Pharm* 41: 791-800.
67. Blasi P, Schoubben A, Giovagnoli S, Rossi C, Ricci M (2010) Alginate micro- and nanoparticle production by spray drying. *Proc Meet Lact as a Carr Inhal Prod Parma, Italy*, 137-138.
68. Cerchiara T, Abruzzo A, di Cagno M, Bigucci F, Bauer-Brandl A, et al. (2015) Chitosan based micro- and nanoparticles for colon-targeted delivery of vancomycin prepared by alternative processing methods. *Eur J Pharm Biopharm* 92: 112-119.
69. Jain (2014) Crosslinking albumin for drug release from spray dried particles, Master Thesis, Electronic Thesis and Dissertations, Paper 674," University of Louisville, USA, 2014.
70. Torge A, Grützmacher P, Mücklich F, Schneider M (2017) The influence of mannitol on morphology and disintegration of spray-dried nano-embedded microparticles. *Eur J Pharm Sci* 104: 171-179.
71. Hindle M, Kaviratna A, Yamarthi D, Longest PW (2015) Characterization of Spray Dried Azithromycin Dry Powders for Inhalation. *Journal of Aerosol Medicine and Pulmonary Drug Delivery* 28: A9-A9.
72. Nguyen TV, Nguyen TTH, Wang SL, Vo TPK, Nguyen AD (2017) Preparation of chitosan nanoparticles by TPP ionic gelation combined with spray drying, and the antibacterial activity of chitosan nanoparticles and a chitosan nanoparticle–amoxicillin complex. *Res Chem Intermed* 43: 3527-3537.
73. Merchant Z, Taylor KM, Stapleton P, Razak SA, Kunda N, et al. (2014) Engineering hydrophobically modified chitosan for enhancing the dispersion of respirable microparticles of levofloxacin. *Eur J Pharm Biopharm* 88: 816-829.
74. Rampino A, Borgogna M, Blasi P, Bellich B, Cesàro A (2013) Chitosan nanoparticles: Preparation, size evolution and stability. *Int J Pharm* 455: 219-228.
75. Yang X, Xu Y, Cai Y, Li H (2015) Novel nano-spray-dried powders for efficient pulmonary drug delivery. *J Control Release* 213: e117-e118.
76. Son YJ, Worth Longest P, Hindle M (2013) Aerosolization Characteristics of Dry Powder Inhaler Formulations for the Excipient Enhanced Growth (EEG) Application: Effect of Spray Drying Process Conditions on Aerosol Performance. *Int J Pharm* 443: 137-145.
77. Behara SR, Longest PW, Farkas DR, Hindle M (2014) Development and Comparison of New High-Efficiency Dry Powder Inhalers for Carrier-Free Formulations. *J Pharm Sci* 103: 465-477.
78. Behara SR, Farkas DR, Hindle M, Longest PW (2014) Development of a High Efficiency Dry Powder Inhaler: Effects of Capsule Chamber Design and Inhaler Surface Modifications. *Pharm Res* 31: 360-372.
79. Behara SR, Longest PW, Farkas DR, Hindle M (2014) Development of high efficiency ventilation bag actuated dry powder inhalers. *Int J Pharm* 465: 52-62.
80. Guo J, Li H (2013) Nano spray drying of alkaline phosphatase with β -cyclodextrin and l-leucine for inhalation. *J Control Release* 172: e107.

81. Schoubben A, Giovagnoli S, Tiralti MC, Blasi P, Ricci M (2014) Capreomycin inhalable powders prepared with an innovative spray-drying technique. *Int J Pharm* 469: 132-139.
82. Schoubben, Giovagnoli S, Blasi P, Ricci M (2013) Production of a capreomycin sulfate inhalable powder by nano spray-drying.
83. Gautier S, Arpagaus C, Schaefroth N, Meuri M, Deschamps A et al. (2010) Very fine chitosan microparticles with narrow & controlled size distribution using spray-drying technologies". *Drug Deliv Technol* 10: 30-37.
84. Dahili LA, Nagy E, Feczko T (2017) 2,4-Dichlorophenol Enzymatic Removal and Its Kinetic Study Using Horseradish Peroxidase Crosslinked to Nano Spray-Dried Poly(Lactic-Co-Glycolic Acid) Fine Particles. *J Microbiol Biotechnol* 27: 768-774.
85. Schultz I, Vollmers F, Lühmann T, Rybak JC, Wittmann R, et al. (2015) Pulmonary Insulin-like Growth Factor I Delivery from Trehalose and Silk-Fibroin Microparticles. *ACS Biomater Sci Eng* 1: 119-129.
86. Dimer FA, Ortiz M, Pohlmann AR, Guterres SS (2015) Inhalable resveratrol microparticles produced by vibrational atomization spray drying for treating pulmonary arterial hypertension. *J Drug Deliv Sci Technol* 29: 152-158.
87. Sithole MN, Choonara YE, du Toit LC, Kumar P, Marimuthu T, et al. (2017) Development of a Novel Polymeric Nanocomposite Complex for Drugs with Low Bioavailability. *AAPS PharmSciTech* 6: 1-12.
88. E Al-Dhubiab (2013) Formulation and In Vitro Evaluation of Gelatin Nanospheres for the Oral Delivery of Selegiline. *Curr Nanosci* 9: 21-25.
89. Harsha S, Al-dhubiab BE, Nair AB, Attimarad M, Venugopala KN, et al. (2017) Pharmacokinetics and tissue distribution of microspheres prepared by spray drying technique: Targeted drug delivery. *Biomed Res* 28: 3387-3396.
90. Anzar N, Mirza MA, Anwer K, Khuroo T, Alshetali AS, et al. (2018) Preparation, evaluation and pharmacokinetic studies of spray dried PLGA polymeric submicron particles of simvastatin for the effective treatment of breast cancer. *J Mol Liq* 249: 609-616.
91. Del Gaudio P, Russo P, Rodriguez Dorado R, Sansone F, Mencherini T, et al. (2017) "Submicrometric hypromellose acetate succinate particles as carrier for soy isoflavones extract with improved skin penetration performance. *Carbohydr Polym* 165: 22-29.
92. Del Gaudio P, Sansone F, Mencherini T, De Cicco F, Russo P, et al. (2016) Nanospray Drying as a Novel Tool to Improve Technological Properties of Soy Isoflavone Extracts. *Planta Med* 83: 426-433.
93. Zellnitz S, Schroettner H, Urbanetz NA (2014) Surface modified glass beads as model carriers in dry powder inhalers-influence of drug load on the fine particle fraction. *Powder Technol* 268: 377-386.
94. Zellnitz S, Schroettner H, Urbanetz NA (2015) Influence of surface characteristics of modified glass beads as model carriers in dry powder inhalers (DPIs) on the aerosolization performance. *Drug Dev Ind Pharm* 41: 1710-1717.
95. Arpagaus C, Schaefroth N, Meuri M (2010) Laboratory Scale Spray Drying of Lactose: A Review, *best@buchi Information Bulletin*, Number 57/2010.
96. Pinto JT, Radivojev S, Zellnitz S, Roblegg E, Paudel A (2017) How does secondary processing affect the physicochemical properties of inhalable salbutamol sulphate particles? A temporal investigation. *Int J Pharm* 528: 416-428.
97. Faulhammer E, Zellnitz S, Wutscher T, Stranzinger S, Zimmer A (2018) Performance indicators for carrier based DPIs: Carrier surface properties for capsule filling and API properties for in vitro aerosolization. *Int J Pharm* 536: 326-335.
98. Faulhammer E, Wahl V, Zellnitz S, Khinast JG, Paudel A (2015) Carrier-based dry powder inhalation: Impact of carrier modification on capsule filling processability and in vitro aerodynamic performance. *Int J Pharm* 491: 231-242.
99. Martena V, Censi R, Hoti E, Malaj L, Di Martino P (2012) Indomethacin nanocrystals prepared by different laboratory scale methods: Effect on crystalline form and dissolution behavior. *J Nanoparticle Res* 14: 12.
100. Rascioni R, Censi R, Malaj L, Di Martino P (2016) Effect of particle size reduction and crystalline form on dissolution behaviour of nimesulide. *J Therm Anal Calorim* 123: 2213-2223.
101. Lee SH, Teo J, Heng D, Ng WK, Chan HK, et al. (2013) Tan Synergistic combination dry powders for inhaled antimicrobial therapy: Formulation, characterization and in vitro evaluation. *Eur J Pharm Biopharm* 83: 275-284.
102. Harsha SN, Aldhubiab BE, Nair AB, Alhaider IA, Attimarad M, et al. (2015) Nanoparticle formulation by Büchi B-90 Nano Spray Dryer for oral mucoadhesion. *Drug Des Devel Ther* 9: 273-282.
103. Sree Harsha N, Bander E Aldhubiab, Ibrahim Abdulrahman Alhaider, Mahesh Attimarad, Anroop Nair (2013) Carbopol 934-P loaded with vildagliptin for diabetic delivery: In Vitro and In Vivo Evaluation of Nanoparticles. *Curr Nanoscience* 9: 642-647.
104. Harsha N (2015) "In Vitro and In Vivo Evaluation of Nanoparticles Prepared by Nano Spray Drying for Stomach Mucoadhesive Drug Delivery. *Dry Technol* 33: 1199-1209.
105. Harsha S, Al-Dhubiab BE, Nair AB, Al-Khars M, Al-Hassan M, et al. (2015) Novel Drying Technology of Microsphere and Its Evaluation for Targeted Drug Delivery for Lungs. *Dry Technol* 33: 502-512.
106. Harsha S, Al-Khars M, Al-Hassan M, Kumar NP, Nair AB, et al. (2014) Pharmacokinetics and tissue distribution of spray-dried carboplatin microspheres: Lung targeting via intravenous route. *Arch Pharm Res* 37: 352-360.
107. Zernov AL, Bonartsev Ap, Yakovlev SG, Myshkina VL, Makhina TK, et al. (2017) Low molecular weight poly(3-hydroxybutyrate) microparticles synthesized by piezoelectric spray drying for the sustained release of paclitaxel. *Nanotechnologies Russ* 12: 218-225.
108. Bonartsev AP, Zernov AL, Yakovlev SG, Zharkova II, Myshkina VL, et al. (2017) New Poly(3-hydroxybutyrate) Microparticles with Paclitaxel Sustained Release for Intraperitoneal Administration. *Anticancer Agents Med Chem* 17: 434-441.
109. Nazarov A, Zavarzin I, Nazarov G, Aksenov A, Levina I (2013) Preparation and Bioavailability Evaluation of Micronized Steroidal Mecigestone Drug Substance. *Pharm Chem J* 49: 706-710.