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ORIGINAL RESEARCH ARTICLE

# **Multiple Sclerosis Brain: Beyond Hyperintense Images**

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#### Abstract

**Introduction:** Multiple Sclerosis (MS) is defined as a chronic, inflammatory demyelinating disease of the central nervous system. It has a multifactorial origin and it is characterized by disabling inflammatory attacks in the central nervous system. It affects any functional system (visual, motor, sensory, coordination, language and sphincter control) and it is considered as more disabling not traumatic disease of young population in the world.

**Objective:** Describe brain anatomic changes in a group of MS patients through post-processing image techniques and correlate it with clinic abnormalities.

**Method:** Thirty patients with relapsing-remitting form of MS and thirty healthy subjects were recruited, they were paired in age and sex. T1 and T2 weighted, FLAIR and DTI 3T MRI scans were acquired. Tractography, Voxel Based Morphometry (VBM) and cortical thickness processing analysis were done.

Results: In relation of MS patients, tractography revealed that corticospinal tract and optic radiation number of fibres were lower than healthy subjects (p = 0.02), (p = 0.00). The number of fibres of evaluated tracts does not diminish significantly when disease duration increasing (p = 0.66), (p = 0.07), (p = 0.32). VBM revealed brain atrophy on subcortical areas of frontal and parietal lobes, occipital lobe, periventricular areas, brainstem, pulvinar thalamus and hippocampus; external capsule, extreme capsule, optic radiation, caudal fibres, arcuate fasciculus, fornix, frontal inferior gyrus, corona radiata, subcortical areas of parietotemporo-occipital lobes, corpus callosum head, white matter of pons and medulla oblongata and cingulate gyrus of MS patients. Cortical thickness analysis did not show significantly differences between MS and healthy subjects (p = 0.26). However, it diminished when disease duration increased (p = 0.03).

**Conclusions:** In our MS patient's series was demonstrated morphologic abnormalities of grey and white mater, principally of subcortical and brainstem structures. These abnormalities increase when some clinical aspects get worse.

#### Keywords

Multiple sclerosis, MS, Tractography, Voxel based morphometry, Cortical thickness

# Introduction

According to the International Classification of Diseases eleven edition (ICD11), Multiple Sclerosis (MS, code: 8A40) is defined as a chronic, inflammatory demyelinating disease of the central nervous system [1]. It has a multifactorial origin and it is characterized by disabling inflammatory attacks in the central nervous system [2]. Three categories of multiple sclerosis have been outlined: Relapsing-remitting, secondary progressive and primary progressive multiple sclerosis [1].

It affects any functional system (visual, motor, sensory, coordination, language and sphincter control). It is considered as more disabling not traumatic disease of young population in the world. In recent years there have been a general increase of the disease worldwide [2].

On 2016, prevalence had been reported as 2221 thousands, death 19 thousand and disability adjusted life years (DALYs) 1151 thousands, with male/female ratio of 0.48, worldwide [3].

Mean prevalence in Latin America have been reported as 10.1 cases per 100.000 inhabitants; with range of 0.9 to 77.7 On 2017, in Costa Rica the MS incidence reported was of 8.3 per million [2].

Diagnosis is based on McDonald criteria and it is supported by clinic aspects, MRI and cerebrospinal fluid analysis [4].



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Conventional T2-weighted images are highly sensitive in depicting focal demyelinating lesions but lack histopathologic specificity, such as inflammation, oedema, gliosis, and axonal loss, which are all represented as areas of high signal intensity. Because of this lack of specificity, T2-weighted imaging does not provide information that can be reliably associated with the pathologic substrate and clinical status of the patient [5].

In MS research, new post-processing MRI techniques have demonstrated a high degree of specificity and sensitivity in detecting pathological tissue damage. These techniques include diffusion-weighted imaging (DWI), which plays an important role in highlighting brain microstructural damage not visible when conventional sequences are used [6].

An important clinical application for DWI in demyelinating disease is in establishing a differential diagnosis with other pathologies. In some circumstances, tumefactive inflammatory lesions may mimic a cerebral neoplasm, infectious abscess, or vascular ischemia. And in some specific and rare situations, restricted diffusion can be the first marker for a demyelinating lesion, preceding contrast enhancement and associated with subtle T2-weighted image alterations, in the course of disease [5].

Diffusion tensor imaging (DTI) is a powerful noninvasive technique that can be used to investigate white mater (WM) microstructures. When applied to the brain, this technique has the potential to map the WM integrity and the structural connectivity *in vivo*. In recent years, DTI has been increasingly applied to the brain WM studies in MS [7].

For another hand, other post-processing techniques as voxel based morphometry (VBM), cortical thickness, volumetric analysis, and others have showed interesting changes in brain structures of MS patients [6].

With this research we purpose describe structural changes that characterize brain in a group of MS patients, through post-processing MRI studies.

# **Material and Methods**

# **Subjects**

A total of 30 consecutive relapsing-remitting MS patients were recruited, according to modified McDonald criteria [7]. The control group consisted of 30 healthy subjects.

# **Ethical considerations**

The study protocol was approved by Ethical Committee of Cuban Neuroscience Centre and all of patients and healthy subjects were agree with the evaluation and signed informed consent. All procedures of the study were in accordance with the ethical standards of the institution and with the 1964 Helsinki declaration.

# Inclusion criteria for patient group

- Meet the modified McDonald criteria for MS [7].
- Relapsing-remitting form.
- Age upper 20-years-old.
- Both sexes.
- Any race.
- No evidence of other neurologic disease.
- Any disease duration.

# Inclusion criteria for healthy subject group

- No antecedent of disease.
- Age similar to MS group.
- Both sexes.
- Any race.

# Exclusion criteria for patient and healthy group

- Patients with contraindication for MRI.
- Patients that deny participating on the research.

#### Image acquisition

MRI was carried out using a 3T Allegra system scanner (Siemens) device with a standard quadrature head coil.

High-resolution three-dimensional whole-brain T1weighted MRI scans were acquired using a volumetric three-dimensional spoiled fast gradient echo with the following parameters: repetition time (TR) = 2000 ms, echo time (TE) = 2.6 ms, inversion time (TI) = 900ms, slice thickness = 1.0 mm; flip angle = 9 Ê, field of view (FOV) = 230 × 230 mm,  $1 × 1 × 1 mm^3$  voxel size. The volume consisted of 192 contiguous coronal sections covering the entire brain, acquisition matrix: 256 × 256, slice thickness: 1.

T2-weighted MRI scans were acquired with TR = 3500 ms, TE = 354 ms.

FLAIR MRI scans were acquired with TR = 5000 ms, TE = 353 ms, TI = 1800 ms.

DWI data were acquired using a diffusion weighted spin echo imaging sequence with the following parameters: 80 volumes, slice thickness 2.0 mm, representing 80 gradient directions, FOV = 230 mm, TR = 86 ms, TE = 8000 ms, slice thickness = 2.0 mm; flip angle = 90, b = 1000 s/mm<sup>2</sup> and two scan with gradient 0 (b = 0), resolution was  $1 \times 1 \times 1$ .

# Image processing

DICOM to nifty image format was convert with dcm2nii tool, Chris Rorden's dcm2nii: 4AUGUST2014 32bit (https://www.nitrc.org/projects/dcm2nii/).

DTI processing: DTI images were processed using DSI Studio software tool (https://dsi-studio.labsolver.org/).

Images were reoriented into oblique axial, slices were aligned parallel to the anterior-posterior commissural axis with the origin set to the anterior commissure, Eddy currents distortions were corrected, diffusion tensor was estimated, scalar maps were constructed, fibre tracking was done, tensor were visualized and tractography based analysis (automatic) was done.

Based on Montreal neurologic Institute (MNI) maps, ROIs was placed at left (cortico spinal tract, arcuate fascicle and optic radiation) with a volume size of 2.7e+04 mm cubic. An ROI was placed at right (cortico spinal tract, arcuate fascicle and optic radiation) with a volume size of 2.9e+04 mm cubic. A seeding region was placed at whole brain. The anisotropy threshold was randomly selected. The change threshold was 20%. The angular threshold was randomly selected from 15 degrees to 90 degrees. The step size was randomly selected from 0.5 voxel to 1.5 voxels. Tracks with length shorter than 26.9531 or longer than 269.531 mm were discarded. A total of 50000 seeds were placed.

Once tracts were constructed, the following quantitative metrics were calculated automatically:

- Number of tracts (called too number of fibres or count of fibres): It is the number of streamlines generated by the algorithm (n).
- Tract length or mean longitude: It was calculated by multiplying number of coordinates in the streamlines with the distance between the coordinates. It was calculated trough the following equation:

$$\frac{1}{n} \sum_{i=1}^{i=n} \sum_{t=1}^{t=mi-1} \left\| vi(t) - vi(t+1) \right\|_{2}$$

**n** is the total number of tracks, **vi(t)** is a sequence of 3D coordinates representing the trajectory of a track, **t** is a discrete variable from 1 to mi, where **mi** is the number of the coordinates.

- Tracts volume (in mm cubic): It was calculated by multiplying number of voxels passed by all streamlines with the voxel size (N × voxel volume),
- **N** is the total number.
- Diameter (in mm): It was calculated trough the following equation:

$$2\sqrt{\frac{volume}{\pi \times lenght}}$$

- Total surface area =  $N_s \times \text{voxel spacing}^2$ ,  $N_s$  is number of surface voxels.
- Irregularity: Is conceptually similar to convexity and concavity. It is the opposite of compactness or roundness defined in computer vision. It was calculated trough the following equation:

surface area  $\pi \times diameter \times lenght$ 

- Fractional Anisotropy (FA): It is a scalar measure of the preferential axis of diffusion motion. It is related to the integrity of the myelin, the density and the parallelism of the fibres, it has a value ranged from 0 (isotropic) to 1 (totally anisotropic).
- Mean Diffusivity (MD): It is the average displacement of water within a voxel in the main axes.
- Axial Diffusivity (AD): It quantifies how fast water diffuses along the axonal fibres. It is low on axonal damage.
- Radial Diffusivity (RD): It evaluates the perpendicular component of water diffusion to axons [8].

# Voxel based morphometry (VBM) analysis

VBM was a fully automated, whole-brain technique that enables measurement of regional brain volumes based on voxel-wise comparison of grey and white matter volumes using Statistical Parametric Mapping (SPM8, Welcome Department of Imaging Neuroscience, London, United Kingdom) software, running on Matlab 2017a and the DARTEL registration method. Briefly, the process was as follows: T1-weighted images were segmented by using VBM8 toolbox of SPM, the images were imported in DARTEL, rigidly aligned, and segmented into grey and white matter, the grey and white matter segments were co-registered simultaneously by using the fast diffeomorphic image registration algorithm and the flow fields were created, the flow fields were then applied to the rigidly aligned segments to warp them to the common DARTEL space and then were modulated by using the Jacobian determinants, the modulated images from DARTEL were normalized to the MNI template by using an affine transformation estimated from the DARTEL grey matter template and the a priori grey matter probability map without resampling, before the statistical computations, the images were smoothed with an 10-mm FWHM Gaussian filter.

Grey and white matter of MS patients and healthy subjects were compared using t-test statistical analysis, with p < 0.05.

#### **Cortical thickness processing**

Computational Anatomy Toolbox (CAT), version CAT12.6-rc1 (1430) was used for cortical thickness processing, it runs within SPM12. This software tools are freely available at http://dbm.neuro.uni-jena.de/ cat/.

For pre-processing: T1 images were normalized to a template space and segmented into grey matter (GM), white matter (WM) and cerebrospinal fluid (CSF), after the pre-processing is finished, a quality check was done, after that image data were smoothed and finally the GM images were entering into a statistical model.

Table 1: Clinic characteristics of MS patients and healthy subjects.

|  | MS patients (n = 30)  | Healthy subjects (n = 30) | t/X <sup>2</sup> | p-value |
|--|-----------------------|---------------------------|------------------|---------|
| Age mean and SD in years (range)               | 43.20 ± 14.43 (20-66) | 44.60 ± 12.31 (32-64)     | 0.301            | 0.764   |
| Sex (M/F)                                      | 4/26                  | 10/20                     | 0.895            | 0.370   |
| Disease duration mean and SD in months (range) | 15.42 ± 13.31 (1-48)  | NA                        | NA               | NA      |

**Table 2:** Localization of hyperintense image on T2 weight andFLAIR MRI in MS group of patients.

| Site            | Number of patients | Percent |
|-----------------|--------------------|---------|
| Periventricular | 23/30              | 85.18%  |
| Corpus callosum | 10/30              | 37.03%  |
| Frontal area    | 20/30              | 74.07%  |
| Parietal area   | 21/30              | 77.77%  |
| Temporal area   | 4/30               | 14.81%  |
| Occipital area  | 4/30               | 14.81%  |
| Cerebellum      | 3/30               | 11.11%  |
| Others          | 0/30               | 0%      |

**Processing:** CAT uses a fully automated method that allows the measurement of cortical thickness and reconstruction of the central surface in one step. It uses a tissue segmentation to estimate the white matter (WM) distance and then projects the local maxima (which is

equal to the cortical thickness) onto other grey matter voxels using a neighbouring relationship described by the WMdistance. This projection-based thickness (PBT method) allows the handling of partial volume information, sulcal blurring, and sulcal asymmetries without explicit sulcus reconstruction [9,10].

# **Statistical analysis**

Descriptive statistical measures were applied.

Between groups mean comparison (t-test) was done to compare mean parameters of tractography of MS and healthy subjects.

Regression analysis was done in order to evaluate the relation of number of fibres of all of analysed tracts and cortical thickness value with disease duration.

By group automated analysis (based on t-test) was done for VBM and cortical thickness, maps of signification were construed.

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We applied a statistical threshold of p < 0.05 in all statistical analysis.

#### Results

#### **Clinic aspects**

Clinics aspects of all of participants are described in Table 1.

# Localization of hyperintense lesions on T2 weight and FLAIR images

Table 2 shows more frequent sites of localization of hyperintense lesions on T2 weight and FLAIR images in our MS cases series.

#### Tractography

Tractography revealed that corticospinal tract and optic radiation volume of MS patients is lower than healthy subjects (See Figure 1).

# Comparison of tractography parameters between groups (MS patients and healthy subjects):

**Corticospinal Tract (CST) statistical analysis:** It showed diminish of mean number of tracts (p = 0.02), diameter (p = 0.01), volume (p = 0.02) and area (p = 0.02) of MS patients in relation with healthy subjects (See Table 3).

Arcuate Fascicle (AF) statistical analysis: It showed

diminish of area (p = 0.04) of MS patients in relation with healthy subjects (See Table 3).

**Optic Radiation (OR) statistical analysis:** It showed diminish of mean number of tracts (p = 0.00) area (p = 0.00), volume (p = 0.01), diameter (p = 0.03) and irregularity (p = 0.03) of MS patients in relation with healthy subjects. And it also showed increase of MD (p = 0.02) and AD (p = 0.03) of MS patients in relation with healthy subjects (See Table 4).

#### **Regression analysis**

Analysis of number of tracts in relation with disease duration: It showed that any parameters of tractography were significant in relation with the increase of the disease duration.

# Voxel based morphometry

**Patterns of brain atrophy in grey matter:** We observed reduced grey matter density in MS patients in relation with healthy subjects on subcortical areas of frontal and parietal lobes, occipital lobe, periventricular areas, brainstem, pulvinar thalamus and hippocampus (Figure 2); p < 0.05 was considered statistically significant.

#### Patterns of brain atrophy in white matter

We observed reduced white matter density in MS patients in relation with healthy subjects on external

| Variable         | Healthy subjects | MS       | Т        | р                        |
|------------------|------------------|----------|----------|--------------------------|
| Number of fibres | 1543.8           | 1134.50  | -2.47393 | <b>0.02</b> <sup>*</sup> |
| Mean longitude   | 67.47            | 67.10    | 0.10416  | 0.91                     |
| Diameter         | 33.1             | 28.33    | -2.56604 | 0.01*                    |
| Volume           | 58511.4          | 43412.39 | -2.34646 | 0.02 <sup>*</sup>        |
| Total area       | 115188.9         | 64153.37 | -2.34017 | <b>0.02</b> *            |
| Irregularity     | 11.13            | 17.0     | -1.59677 | 0.12                     |
| FA               | 0.43             | 0.4      | 0.05260  | 0.12                     |
| MD               | 0.86             | 0.90     | 0.11207  | 0.91                     |
| AD               | 1.28             | 1.3      | 0.22382  | 0.82                     |
| RD               | 0.65             | 0.7      | -0.46457 | 0.64                     |

Table 3: Mean comparison of CST parameters between healthy subjects and MS patients.

 Table 4: Mean comparison of arcuate fascicle parameters between healthy subjects and MS patients.

| Variable         | Healthy subjects | MS      | t        | Р                        |
|------------------|------------------|---------|----------|--------------------------|
| Number of fibres | 1407.0           | 1252.6  | -0.91205 | 0.37                     |
| Mean longitude   | 1407.0           | 1252.6  | -0.91205 | 0.47                     |
| Diameter         | 33.6             | 32.3    | -0.53258 | 0.59                     |
| Volume           | 61830.8          | 54361.1 | -0.81180 | 0.42                     |
| Total area       | 129547.0         | 82341.7 | -2.10072 | <b>0.04</b> <sup>*</sup> |
| Irregularity     | 13.1             | 19.1    | -1.63855 | 0.11                     |
| FA               | 0.4              | 0.4     | -0.55466 | 0.58                     |
| MD               | 0.8              | 0.8     | -0.49359 | 0.62                     |
| AD               | 1.2              | 1.2     | -0.41007 | 0.68                     |
| RD               | 0.6              | 0.6     | -0.19441 | 0.84                     |





**Figure 2:** Generic MRI brain slices with superimposed areas showing statistically significant regions of grey matter atrophy (p < 0.05, corrected for multiple comparisons) in a group of 30 MS patients compared with 30 healthy age matched subjects using voxel-based morphometry.

It shows grey matter atrophy on subcortical areas of frontal and parietal lobes, occipital lobe, periventricular areas, brainstem, pulvinar thalamus and hypocamppus. The coloured bar represents the T score.



(p < 0.05, corrected for multiple comparisons) in a group of 30 MS patients compared with 30 healthy age matched subjects using voxel-based morphometry.

It shows white matter atrophy on external capsule, extreme capsule, optic radiation, caudal fibers, arcuate fasciculus, fornix, frontal interior gyrus, corona radiata, subcortical areas of parieto-temporo-occipital lobes, corpus callosum head, white matter of pons and medulla oblongata and cingulate gyrus. The coloured bar represents the T score.

capsule, extreme capsule, optic radiation, caudal fibres, arcuate fasciculus, fornix, frontal inferior gyrus, corona radiata, subcortical areas of parieto-temporo-occipital lobes, corpus callosum head, white matter of pons and medulla oblongata, cingulate gyrus (See Figure 3); p < 0.05 was considered statistically significant.

# **Cortical thickness**

Comparison between groups (MS patients and

**healthy subjects):** In relation with comparison of mean cortical thickness of MS patients and healthy subject. There were not statistic significate areas (p = 0.26) (See Figure 4).

Group statistical analysis of cortical thickness did not show group differences between MS and healthy subjects, p < 0.05 was considered statistically significant and surface-based statistical maps not showing clusters of significant (See Figure 5).



**Figure 4:** Comparison of individual mean cortical thickness between healthy subjects and MS patients. Notice they are not significate differences.



**Figure 5:** Cortical thickness group differences between MS and healthy subjects, p < 0.05. Surface-based statistical maps showing that there are not significant clusters.

| Table 5: Mear | n comparison | of optic I | adiation | parameters | between | healthy | subjects | and MS | patients |
|---------------|--------------|------------|----------|------------|---------|---------|----------|--------|----------|
|---------------|--------------|------------|----------|------------|---------|---------|----------|--------|----------|

| Variable         | Healthy subjects | MS       | t        | Р                 |
|------------------|------------------|----------|----------|-------------------|
| Number of fibres | 703.50           | 348.35   | -3.52128 | 0.00*             |
| Mean longitude   | 67.95            | 64.03    | -0.59472 | 0.55              |
| Diameter         | 24.49            | 19.12    | -2.25740 | 0.03 <sup>*</sup> |
| Volume           | 36135.18         | 19286.69 | -2.78815 | 0.01 <sup>*</sup> |
| Total area       | 75988.13         | 34552.61 | -4.28540 | 0.00*             |
| Irregularity     | 9.69             | 15.71    | -2.29991 | 0.03*             |
| FA               | 0.40             | 0.39     | 0.39752  | 0.69              |
| MD               | 0.90             | 0.95     | 2.40932  | 0.02*             |
| AD               | 1.28             | 1.38     | 2.18533  | 0.03 <sup>*</sup> |
| RD               | 0.73             | 0.71     | 1.04583  | 0.30              |

Table 6: Regression summary for dependent variable: Cortical thickness on MS patients in relation with disease duration.

|                  |        | R = 0.56288009 R <sup>2</sup> = 0.31683400 Adjusted R <sup>2</sup> = 0.25990350 F (1,12 = 5.5653 p < 0.3611 Std Error of estimate: 0.30917 |        |           |        |       |
|------------------|--------|--|--------|-----------|--------|-------|
|                  | b*     | Std Error of b*  | b      | Std Error | t      | Р     |
| Intercept        |        |  | 3.010  | 0.129     | 23.28  | 0.00* |
| Disease duration | -0.562 | 0.238  | -0.015 | 0.006     | -2.359 | 0.03* |

Notice it diminishes as disease duration increase

**Regression analysis:** Analysis of cortical thickness in relation with disease duration.

It showed that cortical thickness diminishes when disease duration increasing (p = 0.03) (See Table 5, Table 6 and Figure 6).

# Discussion

Great number of studies have reported abnormalities of brain of MS patients. Majorities of them on white matter due to MS are considered a primary demyelinating disease. However, in the last decades some researches has described abnormalities on grey matter and cortical areas in MS patients; demonstrating secondary degeneration of brain structures [11].

In relation of tractography our cases series showed that most affected tract was OR and in second order CST. It is according with abnormalities of visual system on MS patients, which could be sub-clinically.

Fox reported a progressive increase of MD with AD unchanged in a group of relapsing remitting MS patients prior to gadolinium enhancement, it provided evidence for impaired myelin integrity at the initial stage of MS [11].

Kolbe showed progressive decrease of FA trough optic radiation and near cortex, it was in relation with amplitude decreased and latency prolongation of multimodal evoked potential [12]. Lower values of FA and MD of CST were observed on MS patients in relation with healthy subject in a study carried out for El-Sourgy and col on 2015 [13]. Elshafey demonstrated decrease of FA with MD increase on corpus callosal regions, periventricular areas, frontal and occipital lobes of MS patients in relation with healthy subjects. The statistical analysis showed more significance of MD in the detection of lesions. Thus being demonstrated that DTI quantitative parameters are good predictors of brain tissue damage [14,15].

DTI parameters have been demonstrated very useful not only inside of MS lesions regions, but also around the lesions, this suggests the existence of an extension of the disease invisible in conventional MRI study [16-21].

Some authors affirm that DTI is able to measure the degree of diseased white matter more accurately than T2 weight imaging and may also detect abnormalities earlier than T2. It may represent an important indicator of neuronal structure and its loss in patients with MS [21].

In our case series, the most affected tract was OR. MD was higher in comparison with healthy subject. It is agreeing with Cheng results; it suggests that OR has an increase of diffusivity, indicating axonal damage [22]. We didn't find significative FA abnormalities between MS patients and healthy subjects.

Gajamange, et al. published their results in relation with optic nerve and tract evaluation: Reduced fibre density and amplitude associated with reduced of FD in MS patients compared to healthy subjects, and



Notice it diminishes as disease duration increase.

they proposed it as a potential early marker of clinical disability in MS [23].

In relation with our findings on VBM, some authors have supported grey and white matter loss on MS patients *in vivo* and also in post-mortem studies. Trapp demonstrated cortical atrophy on early states of MS and this phenomenon can be detected on patients with very low brain white matter lesions. He showed in a post-mortem study that MS patients had significantly decrease of cortical neuronal density, specifically on V layer [24].

Sbardella, et al. on 2013 demonstrated in a VBM analysis done reduced GM volume in patients with respect to healthy subject in the cerebellum, thalamus, subgenual gyrus and middle cingulate cortex, superior frontal gyrus, occipital and temporal cortices bilaterally, it could be in relation with cognitive or motor disability [25].

Rothstein published cortical diminish of grey matter on forebrain parenchyma, thalamus, and hippocampal area. Same abnormalities have been showed in postmortem studies, cortical atrophy appeared to be unrelated to the degree of myelin loss [26].

Prinster, et al. on 2010 showed significantly decreased of grey and white matter volume in a group of remitting relapsing MS group of patients, it involved preferentially the left fronto-temporal cortex and precuneus, as well as the anterior cingulate gyrus and the caudate nuclei bilaterally, and to a minor extent the right frontotemporal cortex and right parietal lobule. The VBM analysis of white matter indicated preferential areas on bilaterally periventricular regions in the temporal lobes, juxtacortical insular regions, extending posteriorly through the internal capsule to the thalami, and to the splenium of the corpus callosum.

They confirmed a direct correlation between disease severity and brain tissue loss (both grey and white matter) in the motor system, while lesion load correlated of brain tissue loss mainly affects highly interconnected subcortical structures, including the caudate nuclei and thalami [27].

VBM is an automated technique for assessing brain structural changes. It detects changes in brain morphology caused by small lesions, quantifies changes in the volume and density of brain tissue. Other VBM analysis have showed grey matter volumes were decreased in the right frontal lobe (superior frontal, middle frontal, precentral, and orbital gyri), right parietal lobe (postcentral and inferior parietal gyri), right temporal lobe (caudate nucleus), right occipital lobe (middle occipital gyrus), right insula, right parahippocampal gyrus, and left cingulate gyrus of MS patients in comparison with healthy subject [28]. Hippocampal areas are common mentioned as affected on VBM analysis for different authors and it has been frequently associated with memory deficits in MS patients [29,30].

In relation with cortical thickness we did not find any significant difference between MS patients and healthy subjects, however the findings are controversial. Some authors have showed significant mean global cortical thickness was reduced in multiple sclerosis patients compared to healthy subjects [31-37] and also local cortical thickness was reduced in some areas: Left and right frontal lobe, left and right parietal lobe, precentral, paracentral, postcentral and posterior cingulate cortices in both hemispheres, entorhinal, parahippocampal areas, pars opercularis, pars orbitalis [32-39]. Others authors have also reported diminish of cortical thickness on visual areas [37].

Sailer, et al. reported that there was a highly significant main effect of disease duration [F (2,59) = 11.51, P = 0.002] over cortical thickness, it is in accordance with our results. They observed that patients with disease duration of < 3 years did not exhibit any significant focal cortical thinning compared with normal control subjects. In patients with disease duration up to 5 years, they observed significant focal atrophy that mainly involved the left and right temporal superior gyrus and sulcus as well as the left and right frontal superior gyrus and sulcus. Patients whose disease duration was > 5 years exhibited pronounced focal atrophy beside the temporal and frontal areas, in the motor cortex of the left and right hemisphere [38,39].

Damjanovic, et al. and other authors have showed a significant reduction of all brain volumes, atrophy of cortical grey and white matter, thalamus and basal gangliain MS patients in relation with healthy subject and they have thought it would be in relation with cognitive impairment [40-43].

Some of these researches have correlationed atrophy of cortical grey matter with cognitive dysfunction in MS patients [40,43,44].

Post-mortem studies have confirmed MRI findings. They are revealed decrease of global cortical thickness, diffuse changes in myelination occurring in non-lesional, apparently normal white and grey matter at the early stages of disease and also extensive axonal damage in acute white matter lesions and normal appearing white matter in the progressive stage of MS [45,46].

Carassiti demonstrated that the total neocortical neurons were  $14.9 \pm 1.9$  billion vs.  $24.4 \pm 2.4$  billion in controls (mean  $\pm$  SD) showing that there were 39% fewer neurons in the neocortex of MS than in controls and also he described that the non-adjusted mean proportion of demyelinated cortex in MS patients was  $40 \pm 13\%$ , occipital cortex (p < 0.001) which was the most severely affected. No association was detected either between the number of cortical neurons and white matter lesion volume (p = 0.11) [45].

In the study done by Boaventure, et al. on 2022 they suggested that the pathological abnormalities affecting lesions consist of major demyelination and severe tissue destruction; in contrast, abnormalities affecting normal appearing tissue mainly consist of axonaldamage and loss and microglial activation, but do not include major demyelination [47].

Undoubtedly those morphologic aspects support physiologic abnormalities that can be observed in MS. In the initial stages of MS, many different components of the adaptive and the innate immunity induce demyelination and neuronal loss. Demyelinating focal plaques of white matter produce focal tissue loss and it is the major contributor to brain atrophy, inflammation may be an important contributor to global tissue loss in early disease stages, as the disease progresses additional mechanisms emerge: Such as microglia activation, meningeal inflammation, iron deposition, oxidative stress and diffuse axonal damage in normal appearing white matter [48,49].

Whole brain atrophy has a significant imaging association with physical disability as measured by Expanded Disability Status Scale (EDSS) score, cortical and thalamic atrophy have been the best predictor of poor cognitive functioning, even when mild impairment was detected, cortical atrophy has been relationed with other symptoms in MS: euphoria, disinhibition, aggression, major depressive disorder, autonomic dysfunction and sexual disorders. Fatigue has been reported to be associated with grey matter atrophy in frontal regions and depressed patients were found to present selective cortical thinning in the fronto-temporal regions, while the frontal thinning was found to be the best predictor for depression in MS patients [48].

The most recently connectivity studies have supports MRI and anatomo-pathologic findings in MS. They have demonstrated disrupted principal network organisation in thalamic, deep nuclei networks and it shows a higher correlation with clinical scores disability. The whole brain white matter network was characterized by reduced total strength, global efficiency and local efficiency in MS compared with healthy subject [50-52].

#### In summary

In our analysis different brain structures were observed affected in ME patients:

**Grey matter:** Subcortical areas of fronto-parietooccipital lobes, hypocampus, periventricular areas, pulvinar, thalami and brainstem.

White matter: Optic radiation, corticospinal tract, arcuate fascicle, external and extreme capsule, fornix, white matter of frontal inferior and cingulate gyrus, corona radiate, subcortical areas of parieto-temporooccipital lobes, corpus callosum head, white matter of pons and medulla oblongata, cingulate gyrus. Axonal degeneration seems to be the primary abnormality of principal's tracts, they show diminish of fibre numbers, diameter, volume, total area, increase of RD and MD. The most affected tract was optic radiation, followed by corticospinal tract.

Cortical thickness appears not affected in ME patients, at least in the first three years of diseases duration, but it diminishes with the disease duration increase.

Advanced methods of MRI provide new insight into pathophysiology of this disease and may serve as an additional prospective marker of disease progression.

#### Conclusion

In our MS patient's series was demonstrated morphologic abnormalities of grey and white mater of subcortical structures and brainstem.

#### **Disclosure Statement**

The authors report no conflicts of interest.

The author reports there are no competing interests to declare.

#### References

- 1. (2022) International classification of diseases 11<sup>th</sup> revision.
- Vásquez-Céspedes J, Fernández-Morales H, Valverde-Espinoza JA, Moraga-López A, Carazo-Céspedes K (2021) Perfil demográfico y clínico de la esclerosis múltiple en Costa Rica: Revisión de la casuística nacional a diciembre de 2017. Neurología Argentina 13: 69-77.
- GBD 2016 Neurology Collaborators (2019) Global, regional, and national burden of neurological disorders, 1990-2016: A systematic analysis for the global burden of disease study 2016. The Lancet Neurology 18: 459-480.
- Thompson AJ, Banwell BL, Barkhof F, Carroll WM, Coetzee T, et al. (2017) Diagnosis of multiple sclerosis: 2018 revisions of the McDonald criteria. The Lancet Neurology 17: 162-173.
- Rueda-Lopes FC, da Cruz LCH, Doring TM, Gasparetto EL (2014) Diffusion-weighted imaging and demyelinating diseases: New aspects of an old advanced sequence. AJR Am J Roentgenol 202: W34-W42.
- Sbardella E, Tona F, Petsas N, Pantano P (2013) DTI measurements in multiple sclerosis: Evaluation of brain damage and clinical implications. Multiple Sclerosis International 2013: 1-11.
- Shu N, Liu Y, Li K, Duan Y, Wang J, et al. (2011) Diffusion tensor tractography reveals disrupted topological efficiency in white matter structural networks in multiple sclerosis. Cereb Cortex 21: 2565-2577.
- 8. Yeh F-C (2020) Shape analysis of the human association pathways. Neuroimage 223: 117329.
- 9. Dahnke R, Yotter RA, Gaser C (2012) Cortical thickness and central surface estimation. Neuroimage.
- 10. Dahnke R, Ziegler G, Gaser C (2012) Local adaptive segmentation. HBM.
- Fox RJ, Ontaneda D, Wang X, Sakaie K, Lin J, et al. (2010) Identifying the start of multiple sclerosis tissue injury: A longitudinal DTI study. Proc. Intl. Soc. Mag. Reson. Med 18.

- 12. Kolbe S, Bajraszewski C, Chapman C, Nguyen T, Mitchell P, et al. (2012) Diffusion tensor imaging of the optic radiations after optic neuritis. Hum Brain Mapp 33: 2047-2061.
- El-Sourgy L, Ahmad N, El-Rakhawy M, Gomaa M, Hegazi MA (2015) Applications of MR fiber tractography imaging in multiple sclerosis. The Egyptian Journal of Radiology and Nuclear Medicine 46: 449-454.
- Elshafey R, Hassanien O, Khalil M (2014) Diffusion tensor imaging for characterizing white matter changes in multiple sclerosis. The Egyptian Journal of Radiology and Nuclear Medicine 45: 881-888.
- 15. Asaf A, Evan S, Anat A (2015) Injury to white matter tracts in relapsing-remitting multiple sclerosis: A possible therapeutic window within the first 5 years from onset using diffusion-tensor imaging tract-based spatial statistics. Neuroimage Clin 8: 261-266.
- Commowick O, Fillard P, Clatz O, Warfield SK (2008) Detection of DTI white matter abnormalities in multiple sclerosis patients. Med Image Comput Comput Assist Interv 11: 975-982.
- Bakshi R, Thompson AJ, Rocca MA, Pelletier D, Dousset V, et al. (2008) MRI in multiple sclerosis: Current status and future prospects. Lancet Neurol 7: 615-625.
- Azab AO, Samir HM, El-Basmy AA, Fady M, Shaker FM (2016) Role of MRI diffusion tensor imaging in assessment of normal appearing white matter in cases of multiple sclerosis. Med.J.CairoUniv 84: 33-42.
- 19. Kuchling J, Paul F (2020) Visualizing the central nervous system: Imaging tools for multiple sclerosis and neuromyelitis optica spectrum disorders. Front. Neurol 11.
- Yu HJ, Christodoulou C, Bhise V, Greenblatt D, Patel Y, et al. (2012) Multiple white matter tract abnormalities underlie cognitive impairment in RRMS. Neuroimage 59: 3713-3722.
- Chen J, Zhou C, Zhu L, Yan X, Wang Y, et al. (2017) Magnetic resonance diffusion tensor imaging for occult lesion detection in multiple sclerosis. Exp Ther Med 13: 91-96.
- 22. Chen J, Zhu L, Li H, Lu Z, Chen X, et al. (2016) Diffusion tensor imaging of occult injury of optic radiation following optic neuritis in multiple sclerosis. Exp Ther Med 12: 2505-2510.
- 23. Gajamange S, Raffelt D, Dhollander T, Lui E, van der Walt A, et al. (2018) Fibre-specific white matter changes in multiple sclerosis patients with optic neuritis. NeuroImage: Clinical 17: 60-68.
- 24. Trapp BD, Vignos M, Dudman J, Chang A, Fisher E, et al. (2018) Cortical neuronal densities and cerebral white matter demyelination in multiple sclerosis: A retrospective study. Lancet Neurol 17: 870-884.
- 25. Sbardella E, Petsas N, Tona F, Prosperini L, Raz E, et al. (2013) Assessing the correlation between grey and white matter damage with motor and cognitive impairment in multiple sclerosis patients. PLoS One 8: e63250.
- Rothstein TL (2020) Gray matter matters: A longitudinal magnetic resonance voxel-based morphometry study of primary progressive multiple sclerosis. Front Neurol 11: 581537.
- Prinster A, Quarantelli M, Lanzillo R, Orefice G, Vacca G, et al. (2010) A voxel-based morphometry study of disease severity correlates in relapsing-remitting multiple sclerosis. Mult Scler 16: 45-54.

- Han XM, Tian HJ, Han Z, Zhang C, Liu Y, et al. (2017) Correlation between white matter damage and gray matter lesions in multiple sclerosis patients. Neural Regen Res 12: 787-794.
- 29. Beatriz MB (2015) Cambios estructurales y funcionales del hipocampo en la esclerosis múltiple. Universitat Jaume I.
- 30. Fenu G, Lorefice L, Carta E, Arru M, Carta A, et al. (2021) Brain volume and perception of cognitive impairment in people with multiple sclerosis and their caregivers. Front Neurol 12: 636463.
- Geisseler O, Pflugshaupt T, Bezzola L, Reuter K, Weller D, et al. (2016) Cortical thinning in the anterior cingulate cortex predicts multiple sclerosis patients' fluency performance in a lateralised manner. NeuroImage: Clinical 10: 89-95.
- 32. Baghdadi M, Badwey ME, Khalil M, Dawoud RM (2022) Brain magnetic resonance imaging surface-based analysis and cortical thickness measurement in relapsing remission multiple sclerosis. Egyptian Journal of Radiology and Nuclear Medicine 53.
- 33. Cruz-Gomez AJ, Forero L, Lozano-Soto E, Cano-Cano F, Sanmartino F, et al. (2021) Cortical thickness and serum NfL explain cognitive dysfunction in newly diagnosed patients with multiple sclerosis. Neurol Neuroimmunol Neuroinflamm 8: e1074.
- 34. Dayan M, Rúa SMH, Monohan E, Fujimoto K, Pandya S, et al. (2017) MRI analysis of white matter myelin water content in multiple sclerosis: A novel approach applied to finding correlates of cortical thinning. Front Neurosci 11: 284.
- 35. Narayana PA, Govindarajan KA, Goel P, Datta S, Lincoln JA, et al. (2013) Regional cortical thickness in relapsing remitting multiple sclerosis: A multi-center study. Neuroimage Clin 2: 120-131.
- Palombit A, Castellaro M, Calabrese M, Romualdi C, Pizzini FB, et al. (2017) Cortical thickness variability in multiple sclerosis: The role of lesion segmentation and filling. IEEE 14<sup>th</sup> International Symposium on Biomedical Imaging 792-795.
- Righart R, Schmidt P, Dahnke R, Biberacher V, Beer A, et al. (2017) Volume versus surface-based cortical thickness measurements: A comparative study with healthy controls and multiple sclerosis patients. PLoS One 12: e0179590.
- 38. Sailer M, Fischl B, Salat D, Tempelmann C, Schönfeld MA, et al. (2003) Focal thinning of the cerebral cortex in multiple sclerosis. Brain 126: 1734-1744.
- Tsagkas C, Chakravarty MM, Gaetano L, Naegelin Y, Amann M, et al. (2020) Longitudinal patterns of cortical thinning in multiple sclerosis. Hum Brain Mapp 41: 2198-2215.
- Damjanovic D, Valsasina P, Rocca MA, Stromillo ML, Gallo A, et al. (2017) Hippocampal and deep gray matter nuclei atrophy is relevant for explaining cognitive impairment in MS: A multicenter study. AJNR Am J Neuroradiol 38: 18-24.
- Pontillo G, Cocozza S, Lanzillo R, Russo C, Stasi MD, et al. (2019) Determinants of deep gray matter atrophy in multiple sclerosis: A multimodal MRI study. AJNR Am J Neuroradiol 40: 99-106.
- 42. Eshaghi A, Prados F, Brownlee WJ, Altmann DR, Tur C, et al. (2018) Deep gray matter volume loss drives disability worsening in multiple sclerosis. Ann Neurol 83: 210-222.
- 43. Kletenik I, Alvarez E, Honce JM, Valdez B, Vollmer TL, et al. (2019) Subjective cognitive concern in multiple sclerosis is associated with reduced thalamic and cortical gray matter volumes. Mult Scler J Exp Transl Clin 5: 2055217319827618.

- 44. Kolasinski J, Stagg CJ, Chance SA, Deluca GC, Esiri MM, et al. (2012) A combined post-mortem magnetic resonance imaging and quantitative histological study of multiple sclerosis pathology. Brain 135: 2938-2951.
- 45. Carassiti D, Altmann DR, Petrova N, Pakkenberg B, Scaravilli F, et al. (2018) Neuronal loss, demyelination and volume change in the multiple sclerosis neocortex. Neuropathol Appl Neurobiol 44: 377-390.
- 46. Klaver R, Popescu V, Voorn P, Galis-de Graaf Y, van der Valk P, et al. (2015) Neuronal and axonal loss in normalappearing gray matter and subpial lesions in multiple sclerosis. J Neuropathol Exp Neurol 74: 453-458.
- 47. Boaventura M, Sastre-Garriga J, Garcia-Vidal A, Vidal-Jordana A, Quartana D, et al. (2022) T1/T2-weighted ratio in multiple sclerosis: A longitudinal study with clinical associations. Neuroimage Clin 34: 102967.
- Andravizou A, Dardiotis E, Artemiadis A, Sokratous M, Siokas V, et al. (2019) Brain atrophy in multiple sclerosis: Mechanisms, clinical relevance and treatment options. Auto Immun Highlights 10: 7.

- 49. Calabrese M, Magliozzi R, Ciccarelli O, Geurts JJG, Reynolds R, et al. (2015) Exploring the origins of grey matter damage in multiple sclerosis. Nat Rev Neurosci 16: 147-158.
- 50. Charalambous T, Clayden JD, Powell E, Prados F, Tur C, et al. (2020) Disrupted principal network organisation in multiple sclerosis relates to disability. Sci Rep 10: 3620.
- 51. Cho EB, Kim D, Jeong BC, Shin JH, Chung YH, et al. (2022) Disrupted structural network of inferomedial temporal regions in relapsing-remitting multiple sclerosis compared with neuromyelitis optica spectrum disorder. Sci Rep 12: 5152.
- 52. Tur C, Eshaghi A, Altmann DR, Jenkins TM, Prados F, et al. (2018) Structural cortical network reorganization associated with early conversion to multiple sclerosis. Sci Rep 8: 10715.

